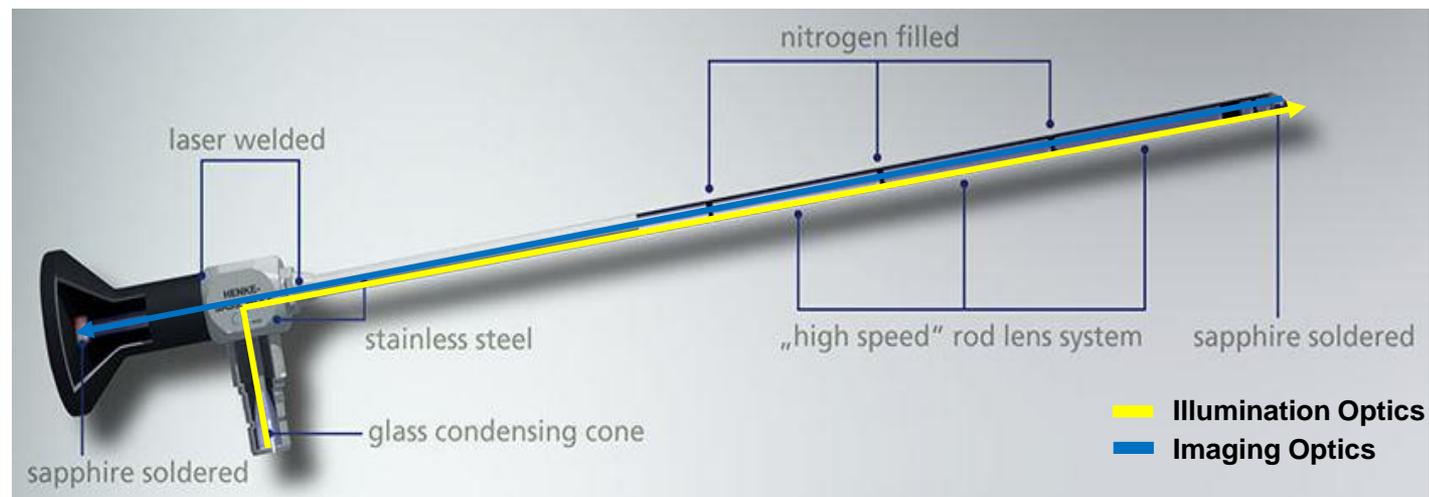
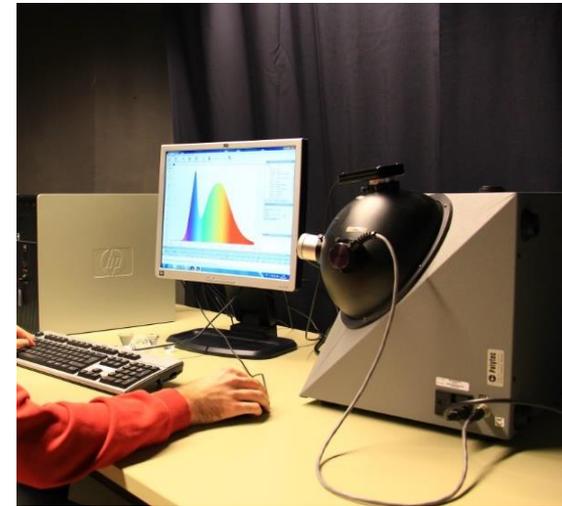
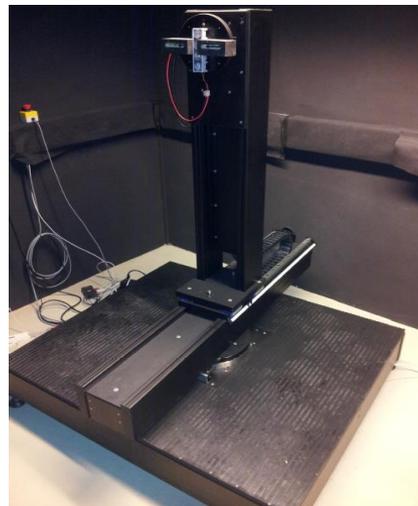
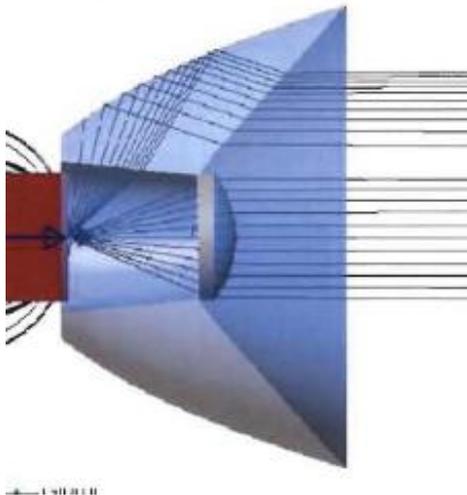


Challenges when designing LED-based illumination systems for medical applications



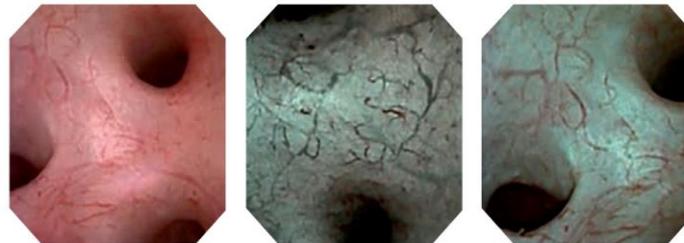
- Introduction
- **Project EDISON**
 - measurements of light sources and endoscopes
 - analysis of intensity losses
 - optical simulations
- Illumination optimised according to reflection properties of human tissues
- **Project Wound Healing**

Lighting Technologies in the Black Forest



State of the Art – Light Sources

- LEDs are systematically replacing Xenon and Halogen lamps in medical devices
 - produce less heat and their spectral emission in the visible range can be tuned
- LED selected with high Ra, mostly R9 (blood) or R13 (skin)
 - but optical properties of biological tissues vary and may be highly reflective (fat), highly absorptive of blue/green light (blood) or may have fluorescent properties (collagen)
- Very few LED-based tunable illumination units available
 - selection criteria of wavelength filtering are not scientifically based



Weißlicht

SPECTRA A

SPECTRA B

Quelle: KARL STORZ; Highlights 2016 - Telepräsenz Bildgebende Systeme, Dokumentation, Beleuchtung, Gerätewagen: "Innovative Visualisierungsmodi in 2D und 3D"; 2016

EdisON



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Bundesministerium
für Bildung
und ForschungFORSCHUNG AN
FACHHOCHSCHULEN

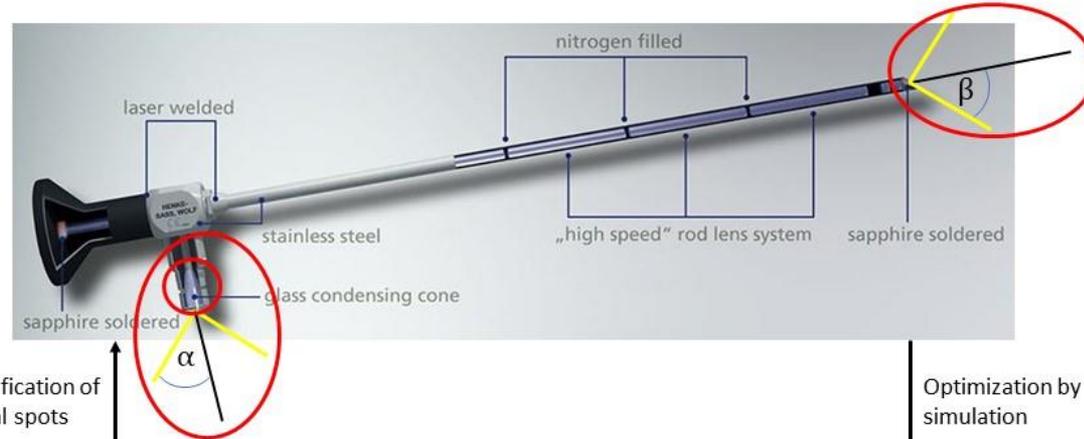
Paola Belloni and Alexander Gärtner

Aim: enhancing efficiency while reducing the volume of the fiber optics inside the endoscope

Standard illumination optics in rigid endoscopes will be redesigned and optimised taking into account constructive and production related boundary conditions.

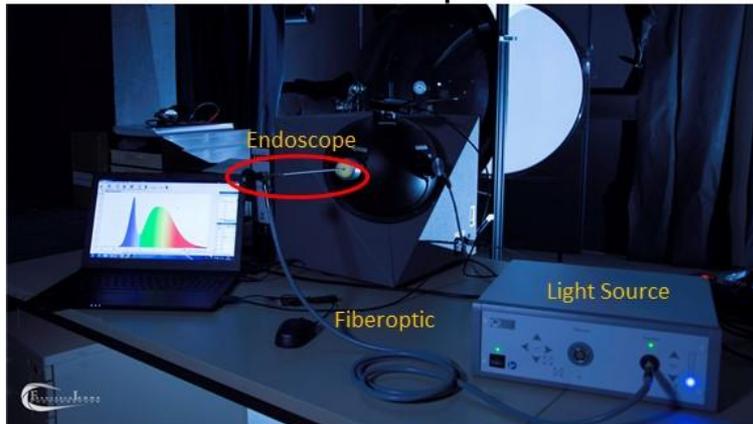
Edison: Project development

Analysis of the optical interfaces and losses

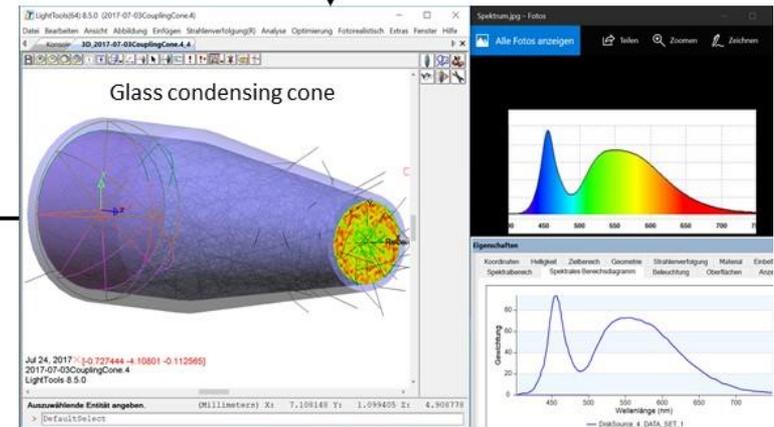


Identification of critical spots

Optimization by simulation



Prototype measurements

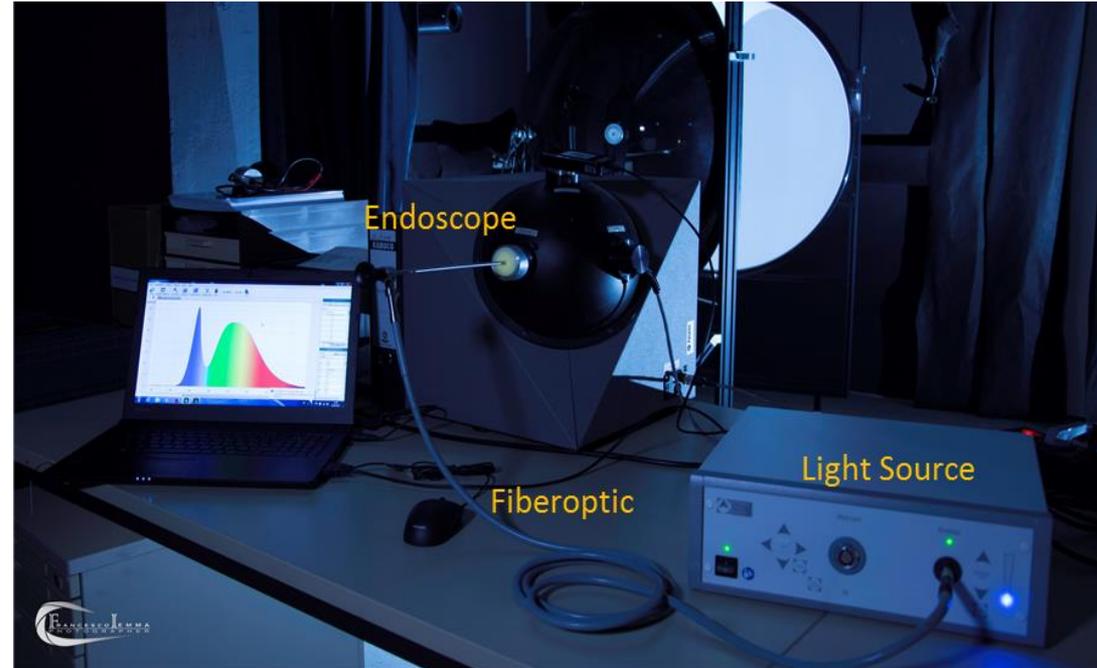


Optical simulations/optimisation

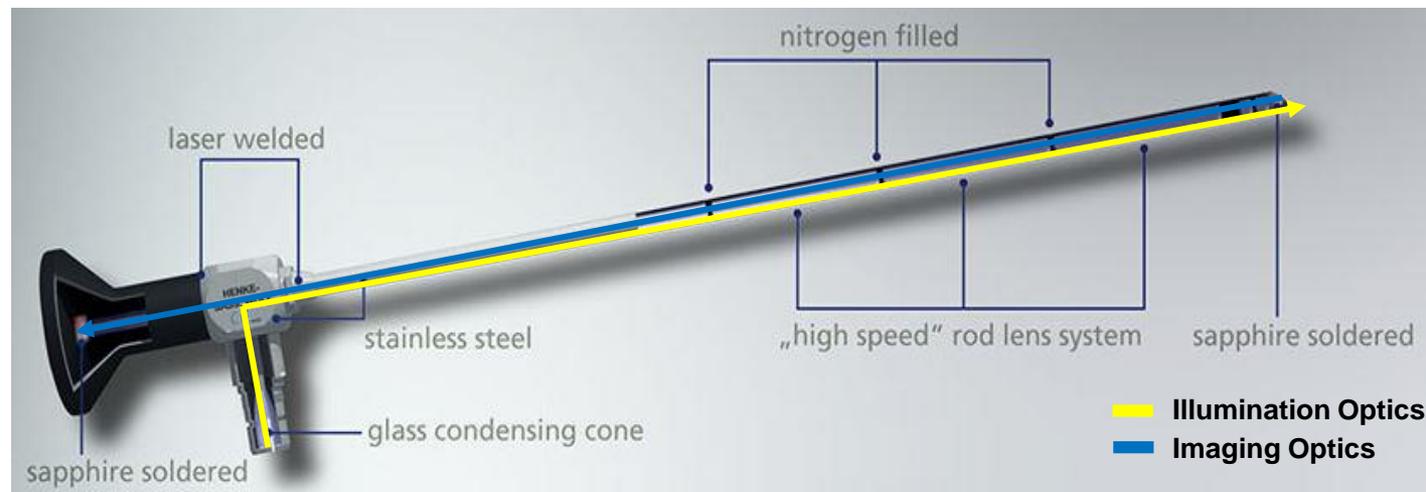
Measurement setup

Equipment:

- Fiberoptic is connected to light source and endoscope
- Endoscope is fixed into auxiliary adapter and mounted on the integrating sphere
- Measurements are performed with an integrating sphere ($\varnothing=25$ cm) and a spectrometer from GL optics



Rigid endoscope with external light sources



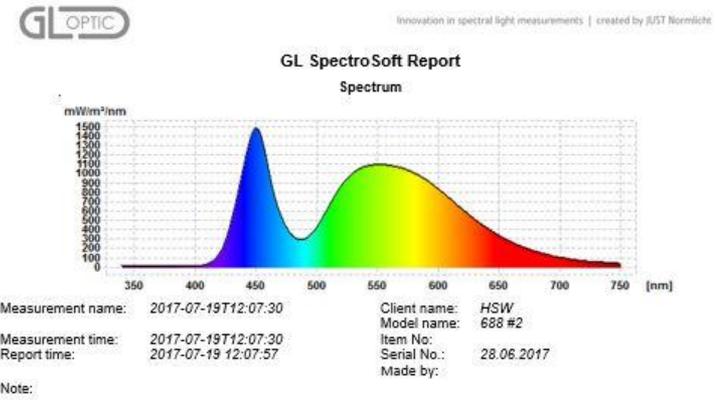
Objectives and measurements

Objectives:

- Identify losses bending the fiber optics inside the endoscope
- Identify losses between the light source input and the endoscope output
- Analyse **three** different **light sources (a,b,c)** and **three** endoscopes

Parameters:

- Illuminance
- Color Temperature
- XY-Chromaticity Coordinates



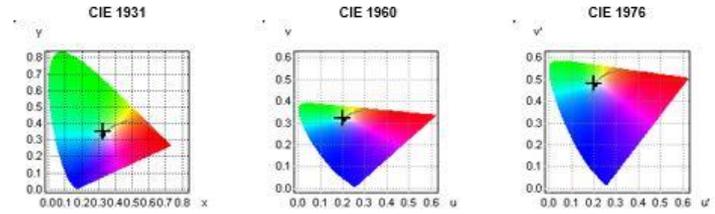
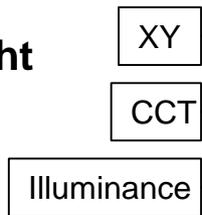
Results

CIE 1931 2°observer		Other		Rendering Indices	
x	0.3256	CCT	5790	Ra	71.0
y	0.3532	Chromaticity Error	0.004	R1	66.5
u'	0.1977	Color Peak	450.47	R2	75.7
v'	0.4928	Color Peak Value	1453.08	R3	81.9
L	68.00	Color Dominant	528.4	R4	70.5
a	-9.47	Luminous Intensity	6408.09	R5	65.0
b	4.42	Purity		R6	67.1
X	59131.72	Radiometric	191.7843	R7	82.5
Y	64153.30	PAR		R8	56.0
Z	58324.79	PPFD		R9	0.0
		Luminous Efficacy		R10	41.8
				R11	65.6
				R12	41.7
				R13	68.1
				R14	89.7

CIE 1984 10°observer	
x	0.3331
y	0.3474
u'	0.2049
v'	0.4808
L	65.54
a	-4.89
b	3.87
X	65499.80
Y	68308.38
Z	62824.64

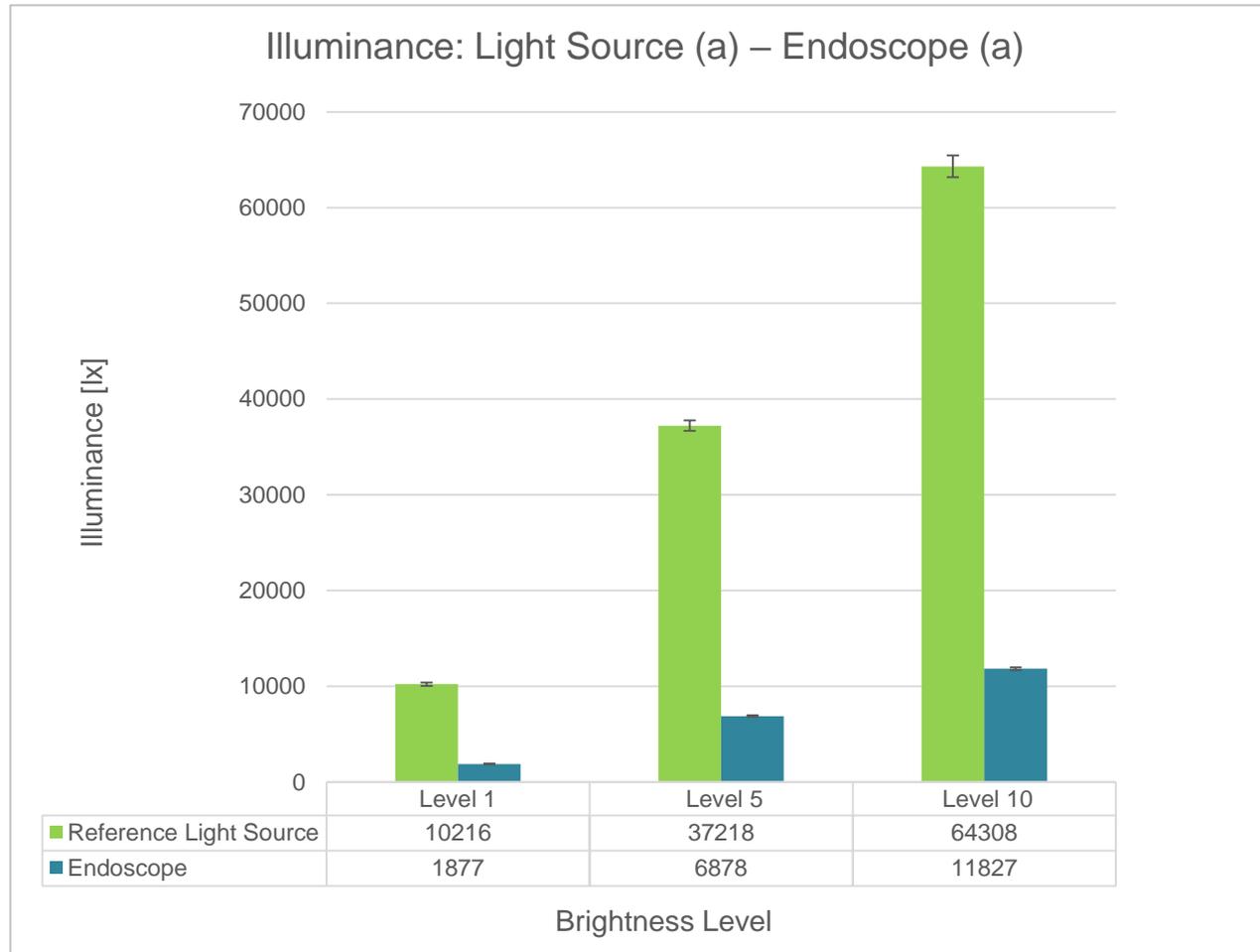
Binning	
Binning	2S
Brightness	

Metamerism Indices	
Miuv	1.9
Miuv	5.8



Parameters extracted from the protocol

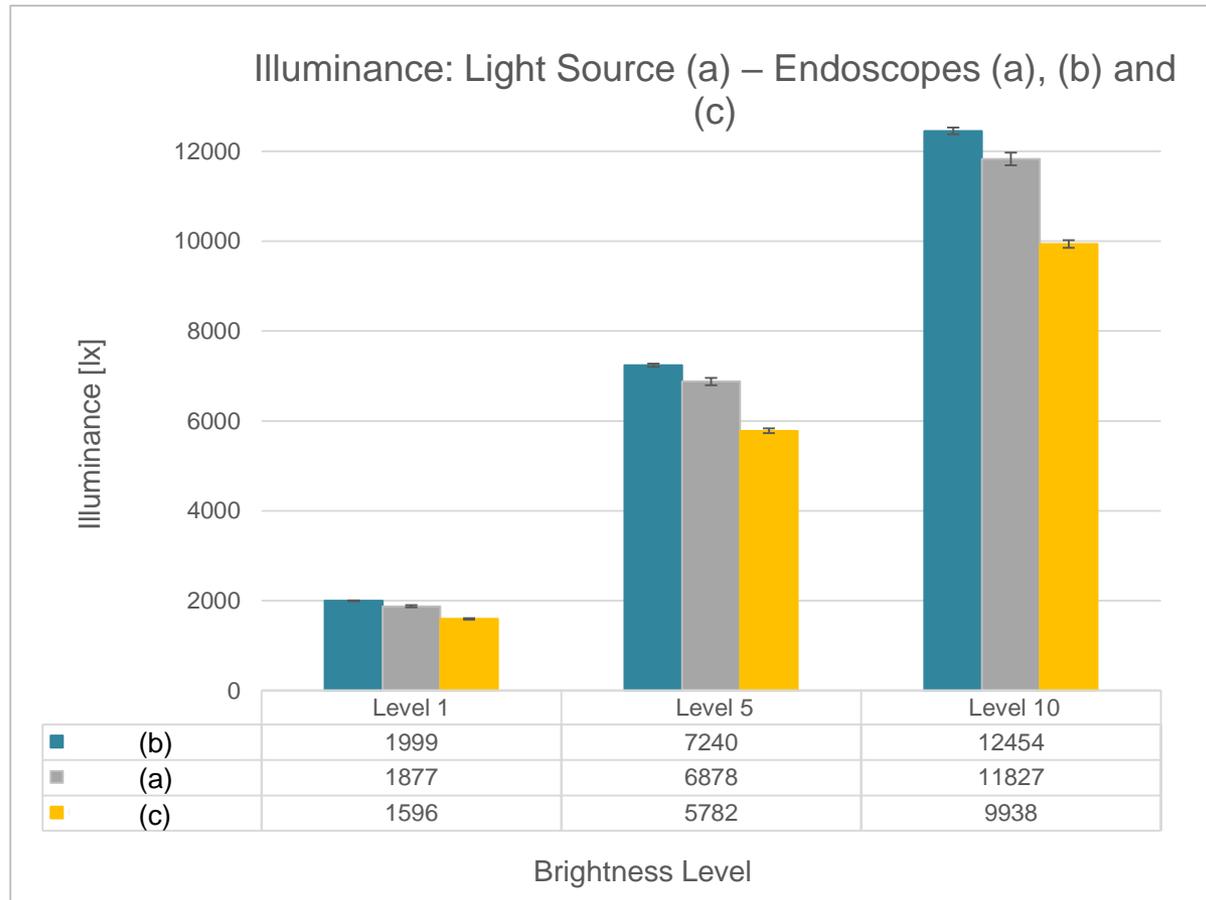
Measurements: Intensity losses



Brightness	Loss [%]
Level 1	81,63
Level 5	81,52
Level 10	81,61

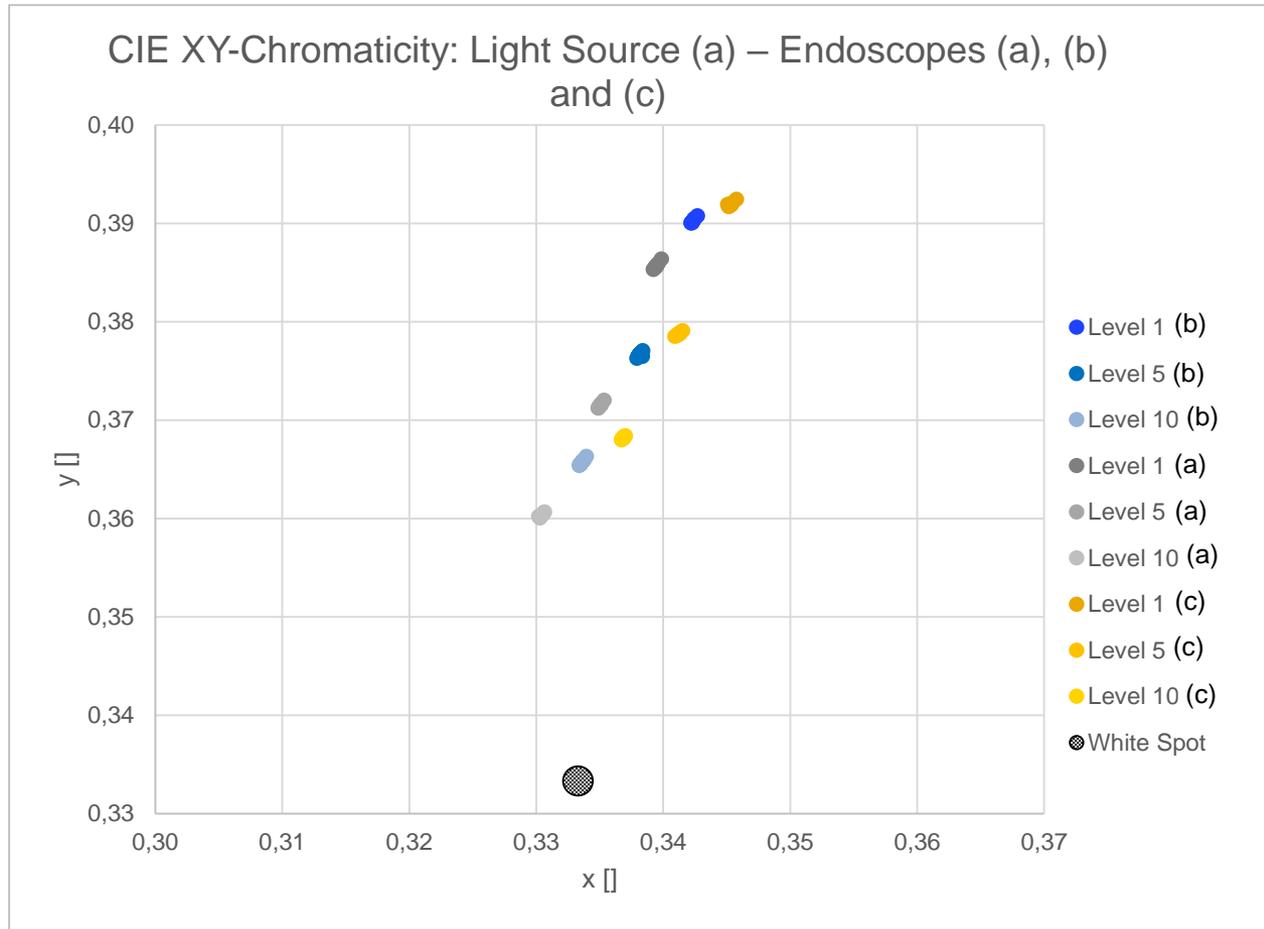
Measurements: Intensity losses

Analysis of additional endoscopes (state of the art)



→ Overall ca **80 %** of the light source intensity is lost before leaving the endoscope !

Measurements: Chromaticity



All endoscopes demonstrate a similar shift changing the brightness levels

Measurements – Fiber bundle

Are intensity losses caused by bending the fiber bundle ?

Analysis of the same fiber bundle used to transport light through the endoscope

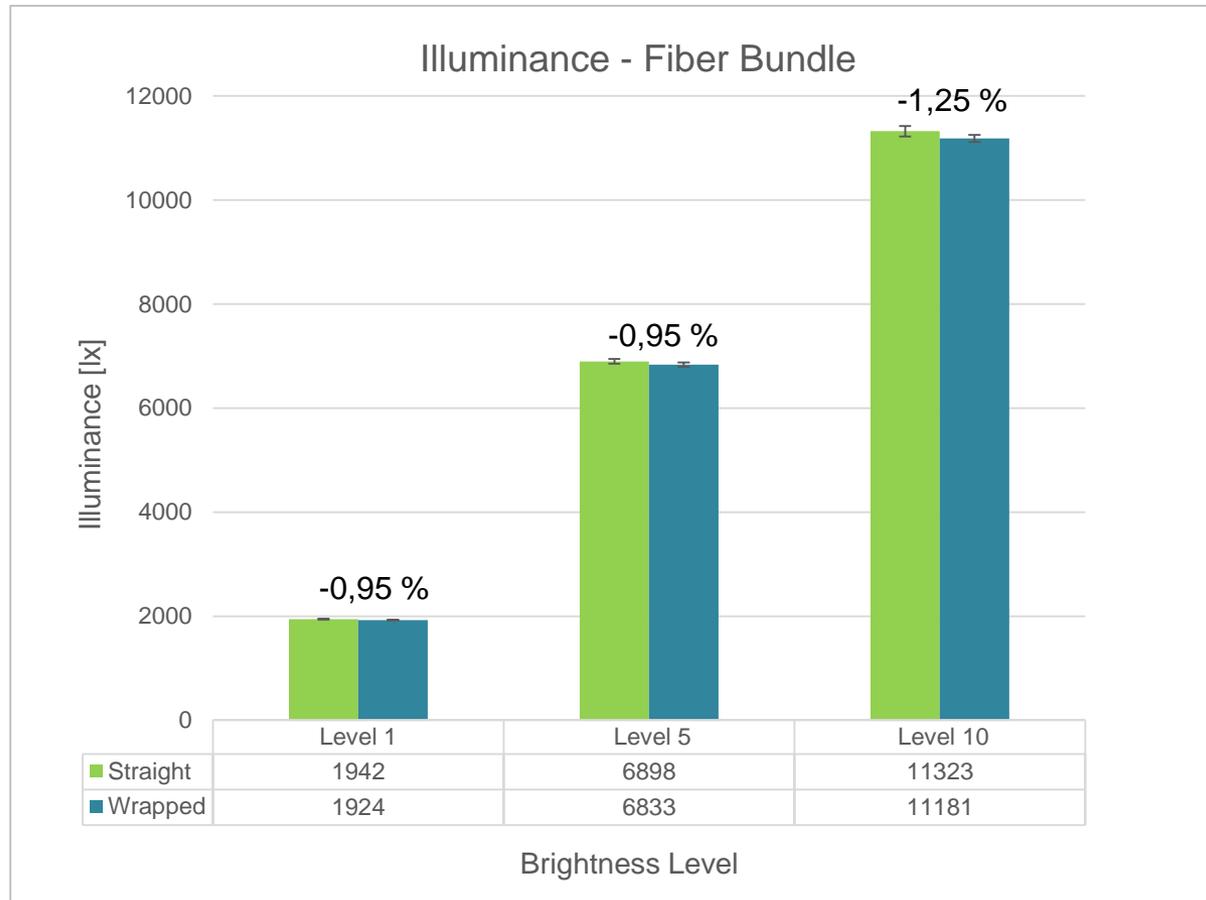
- Measurements of the fiber bundle are performed by holding the fiber straight and wrapped around middle and index finger twice
- 20 measurements are carried out for each brightness level

→ NO perceivable changes in intensity or chromaticity shift



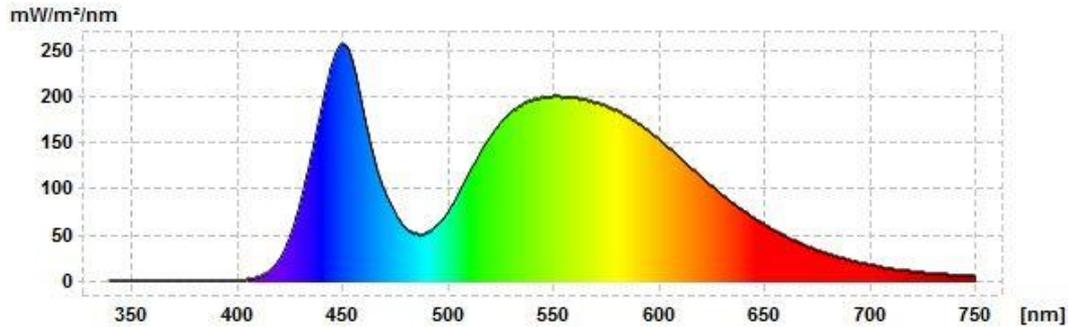
Measurements – Fiber bundle

- Results only show minor (negligible) changes (measurement inaccuracies <4 %)
- 10 measurements per bar are carried out

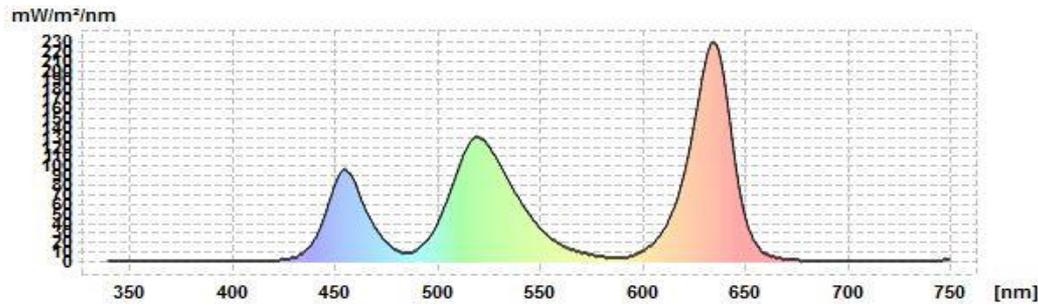


Measurements – Light Sources

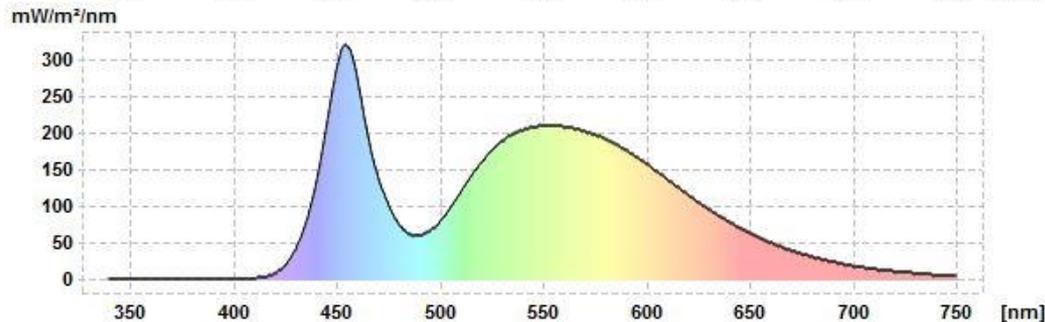
Very different spectral distribution (CCT, Ra, R9 etc..)



Light Source (a)

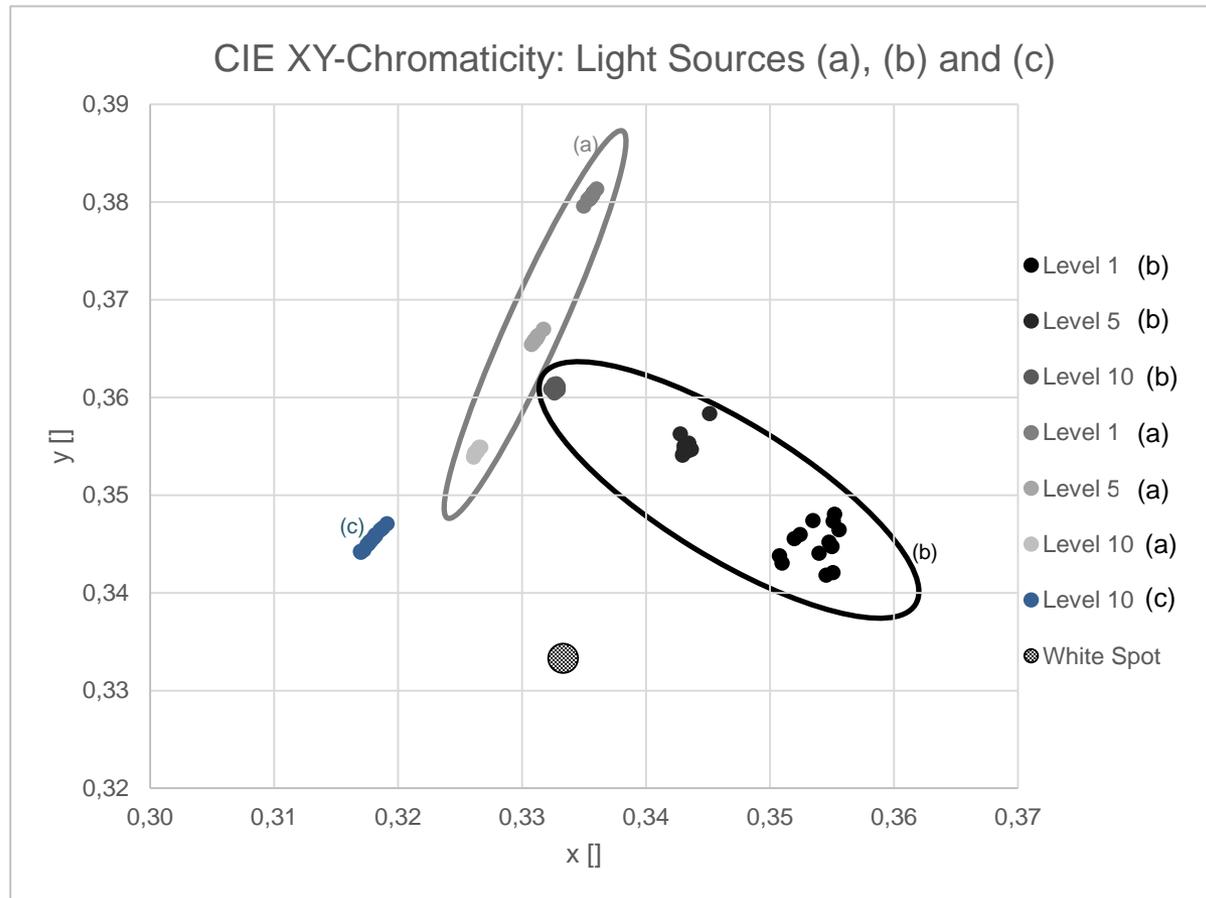


Light Source (b)

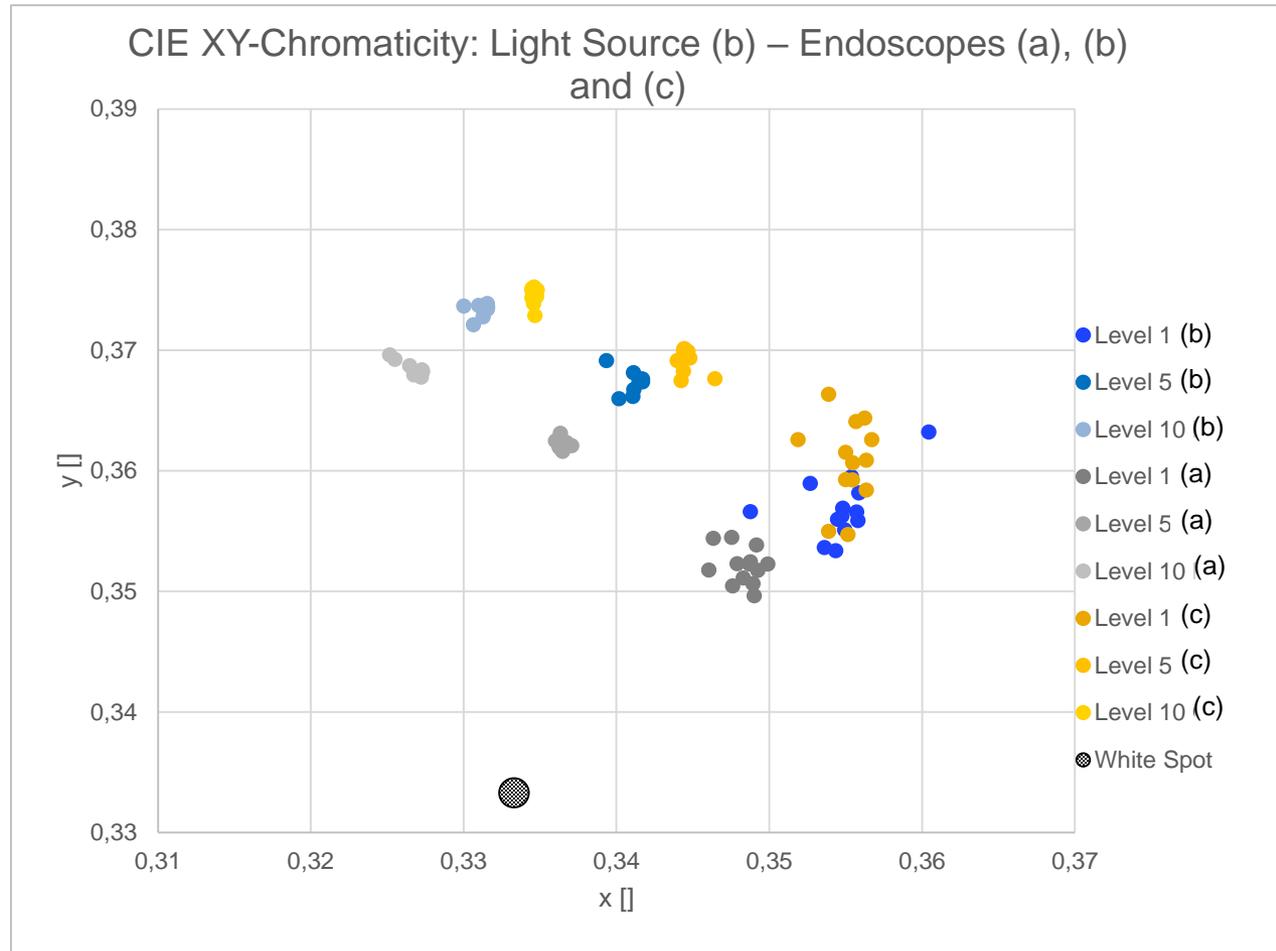


Light Source (c)

Measurements – Chromaticity light sources

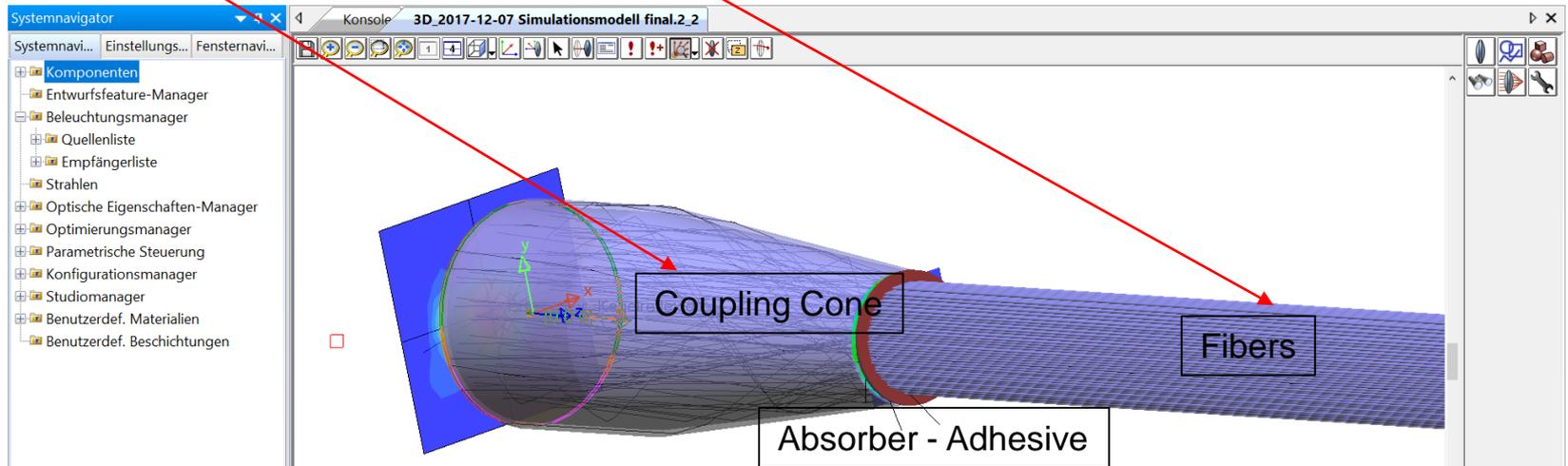
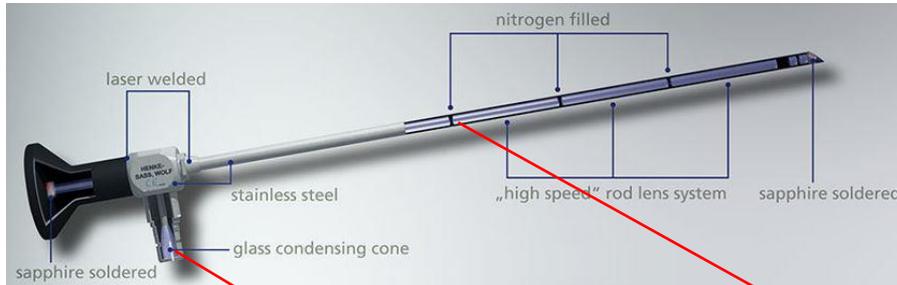


- Stronger x-shift for RGB-light source and high scattering for smaller brightness levels



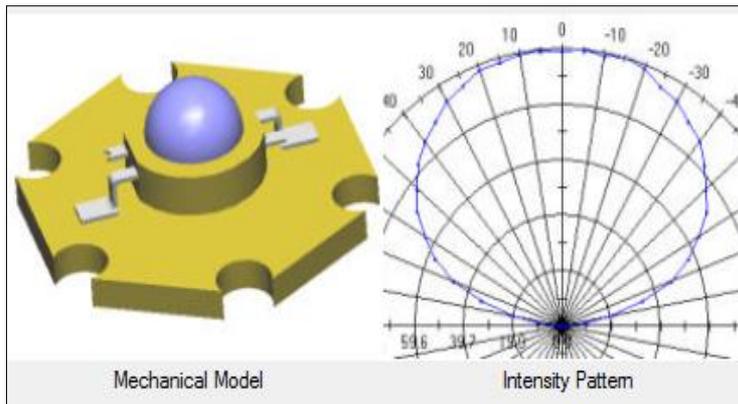
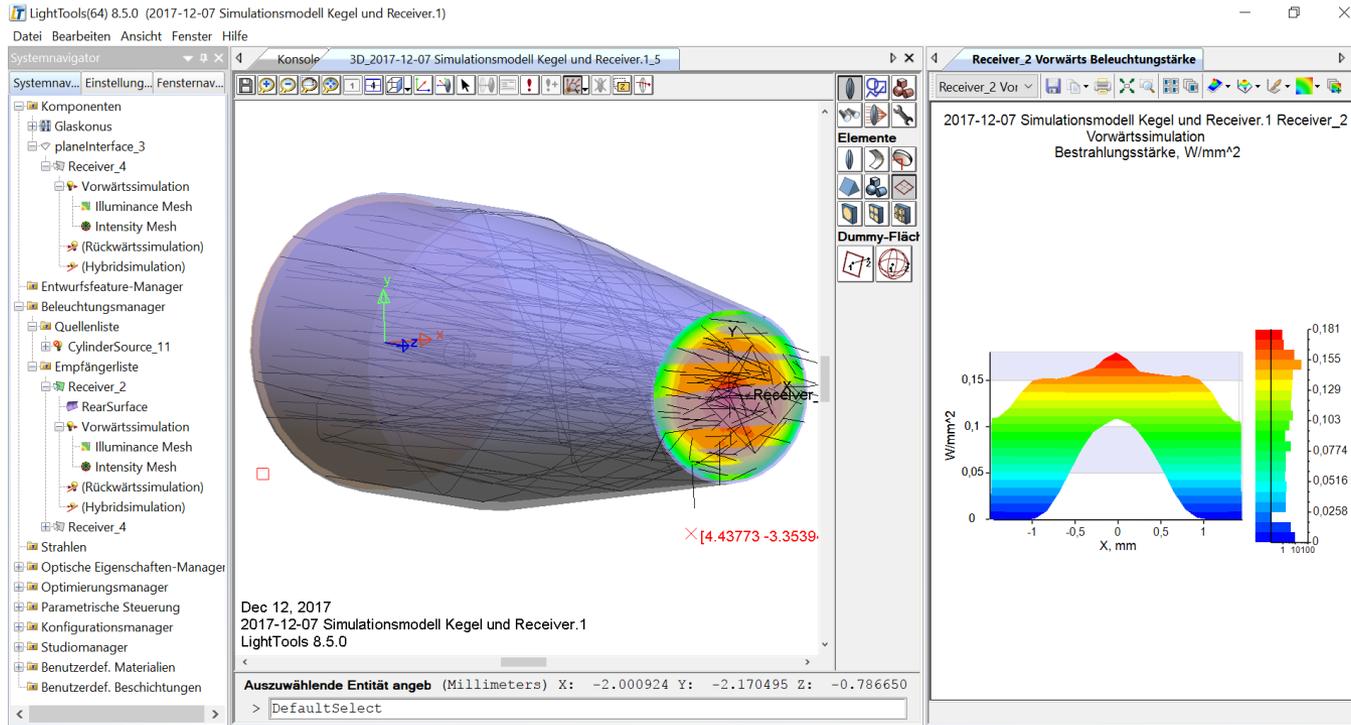
Bigger scattering for lower brightness levels of RGB-light source

Analysis of all critical interfaces for **light coupling** and **transport**



Software LightTools (Synopsis©)

Optical simulations – Light coupling



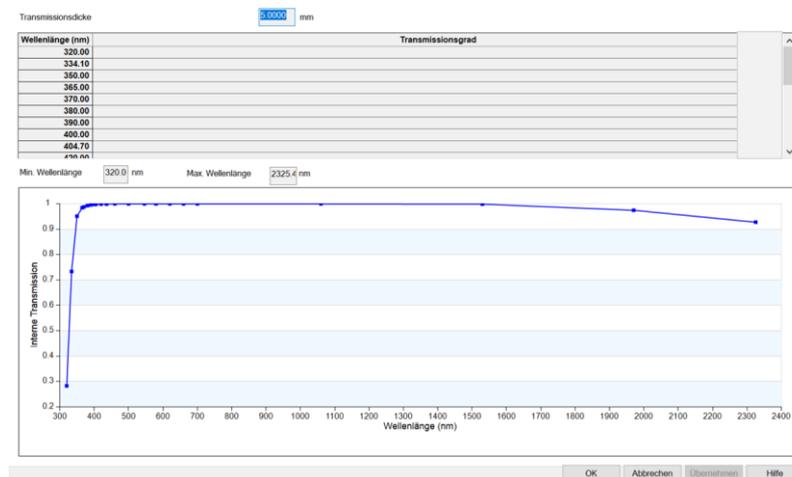
Intensity and uniformity of the light coupling is very much dependent on the light curve distribution (LCD) of the light source

Optical simulations – Light transport

Simulation of fiber bundle : Geometry and optical transmission properties

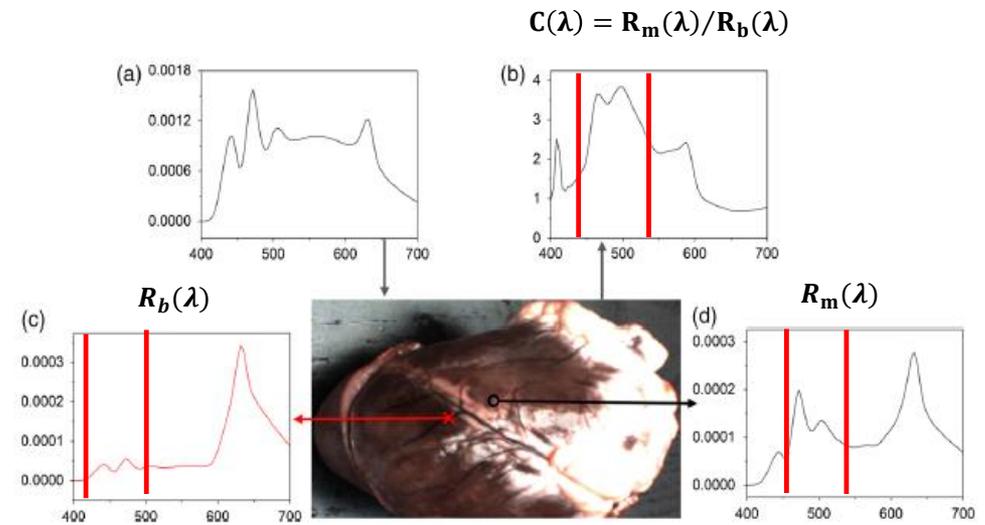
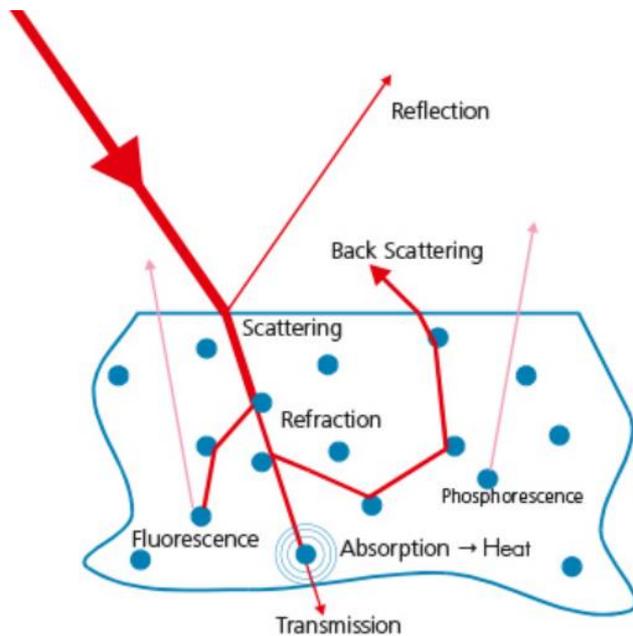
	x-Referenz	y-Referenz	Maximale Höhe	Radius	Zellendrehung
1302	0.57123	-1.0490	0.030000	0.030000	0.00000
1303	-0.51823	-1.0761	0.030000	0.030000	0.00000
1304	0.51823	-1.0761	0.030000	0.030000	0.00000
1305	-0.46395	-1.1006	0.030000	0.030000	0.00000
1306	0.46395	-1.1006	0.030000	0.030000	0.00000
1307	-0.40851	-1.1224	0.030000	0.030000	0.00000
1308	0.40851	-1.1224	0.030000	0.030000	0.00000
1309	-0.35206	-1.1413	0.030000	0.030000	0.00000
1310	0.35206	-1.1413	0.030000	0.030000	0.00000
1311	-0.29473	-1.1575	0.030000	0.030000	0.00000
1312	0.29473	-1.1575	0.030000	0.030000	0.00000
1313	-0.23667	-1.1707	0.030000	0.030000	0.00000
1314	0.23667	-1.1707	0.030000	0.030000	0.00000
1315	-0.17802	-1.1811	0.030000	0.030000	0.00000
1316	0.17802	-1.1811	0.030000	0.030000	0.00000
1317	-0.11892	-1.1885	0.030000	0.030000	0.00000
1318	0.11892	-1.1885	0.030000	0.030000	0.00000
1319	-0.059536	-1.1929	0.030000	0.030000	0.00000
1320	0.059536	-1.1929	0.030000	0.030000	0.00000
1321	-1.7193e-014	-1.1944	0.030000	0.030000	0.00000

Less than 3 % of the input light is absorbed in the 300 mm length



Reflection properties of human tissues

- Physical interaction between light and human tissue is complex
- **Only reflected light** will be captured by a camera system or directly seen by the surgeon
- Reflection properties of the target tissues and their environment must be known
- Color and intensity contrast can be optimised

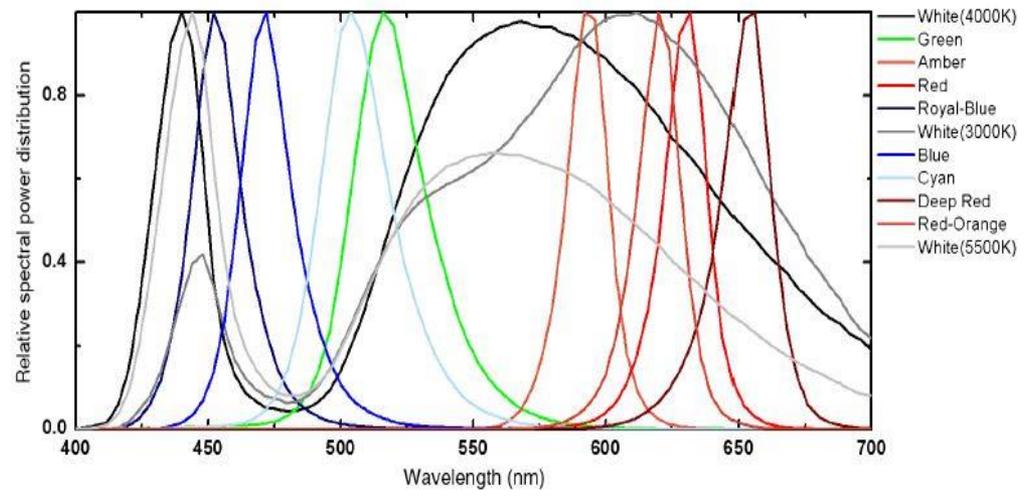


Color contrast $C(\lambda)$ optimised

Quelle: J. Shen, H. Wang, Y. Wu, A. Li, C. Chen, Z. Zheng.: "Surgical lighting with contrast enhancement based on spectral reflectance comparison and entropy analysis" in Journal of biomedical optics 20(10), 105012-2015

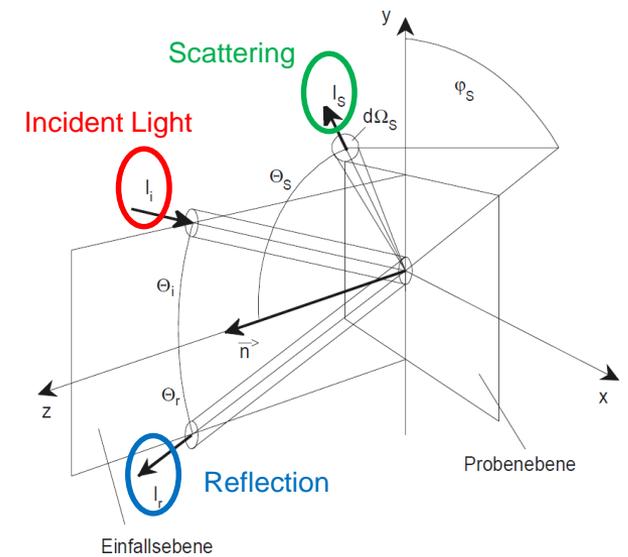
Ongoing research project

Development of a multispectral illumination units which spectral characteristics can be flexibly adapted to the specific diagnostic procedures



Quelle: Huihui Wang, Raymond H. Cuijpers, Ingrid M. L. C. Vogels, Ingrid Heynderickx, Ming Ronnier Luo, Zhenrong Zheng. 17-3: Simultaneous Optimization of Color Contrast and Color Rendering Index for Surgical Lighting. In: Journal of Biomedical Optics 20(1), 015005 (January 2015)

Measurements of bidirectional reflection distribution functions (BRDF) of representative biological tissues



- EX-vivo? IN-vivo?
- How to categorize human tissues? (liver, lung, nerves, fat)

Prototype of an automated photobiomodulation treatment device for in vitro **wound healing** studies

Jacquelyn Dawn Parente, Knut Möller, Paola Belloni, Margareta Müller

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und Forschung



Chronic wounds are a healing process dysfunction

3+ months

Pressure ulcer

Venous leg ulcer

Diabetic foot ulcer

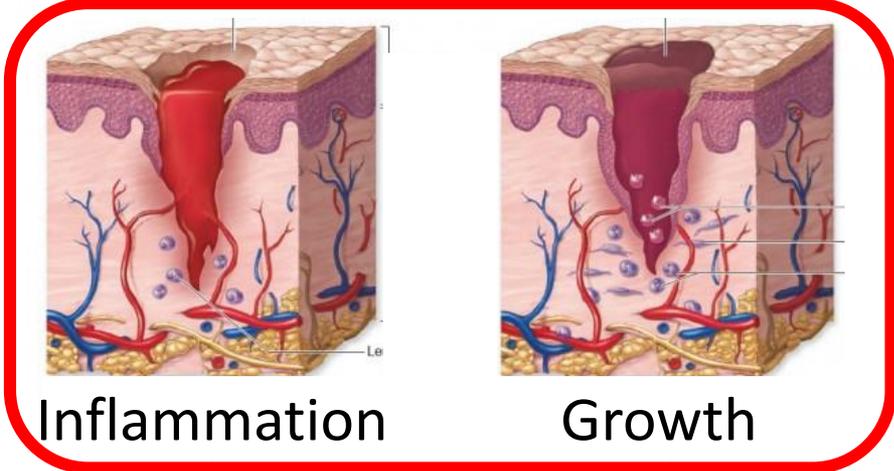


In Germany (2014)

800K diagnosis

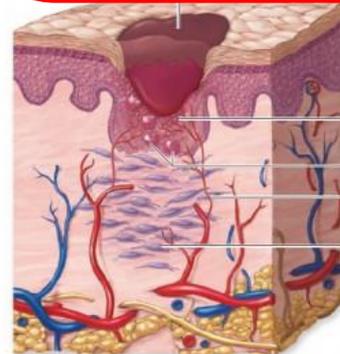
200K new diagnosis

500K treated

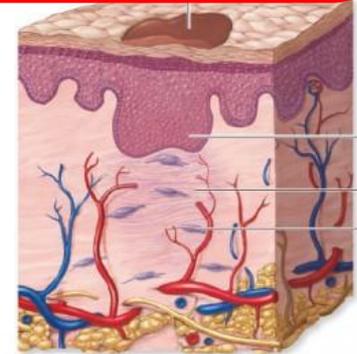


Inflammation

Growth



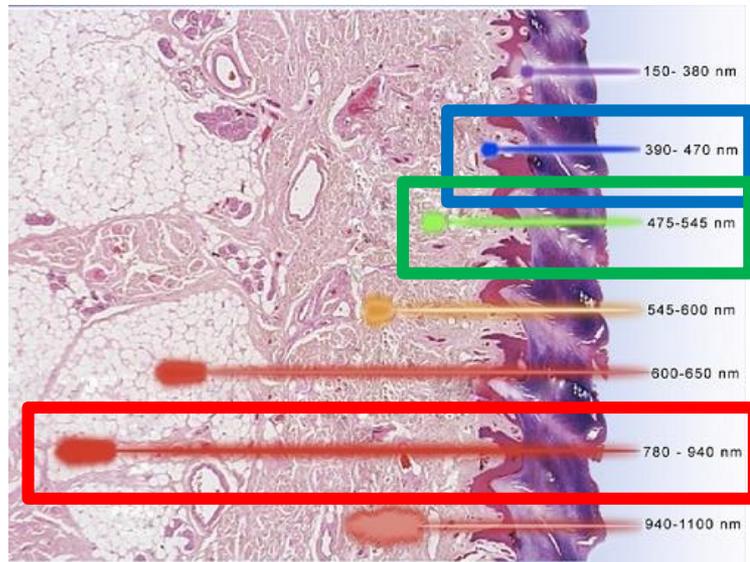
Blood vessels



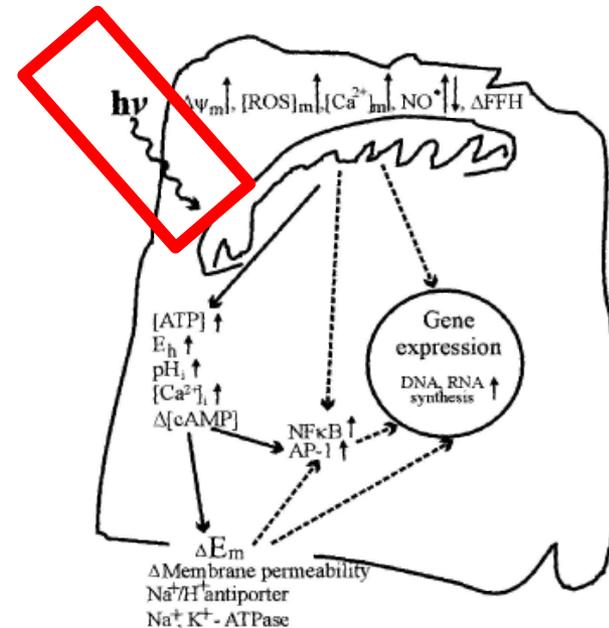
Remodeling

FOCUS: Light therapy re-activates healing processes

Light (LED or LASER)



Photobiomodulation



Wavelength-dependent absorption at mitochondria.

Treatment parameter reporting is unverified

Literature reporting (2015)

1) Wavelength

3% no ,medicine'

2) Irradiance [mW/m^2]

43% no ,dose'

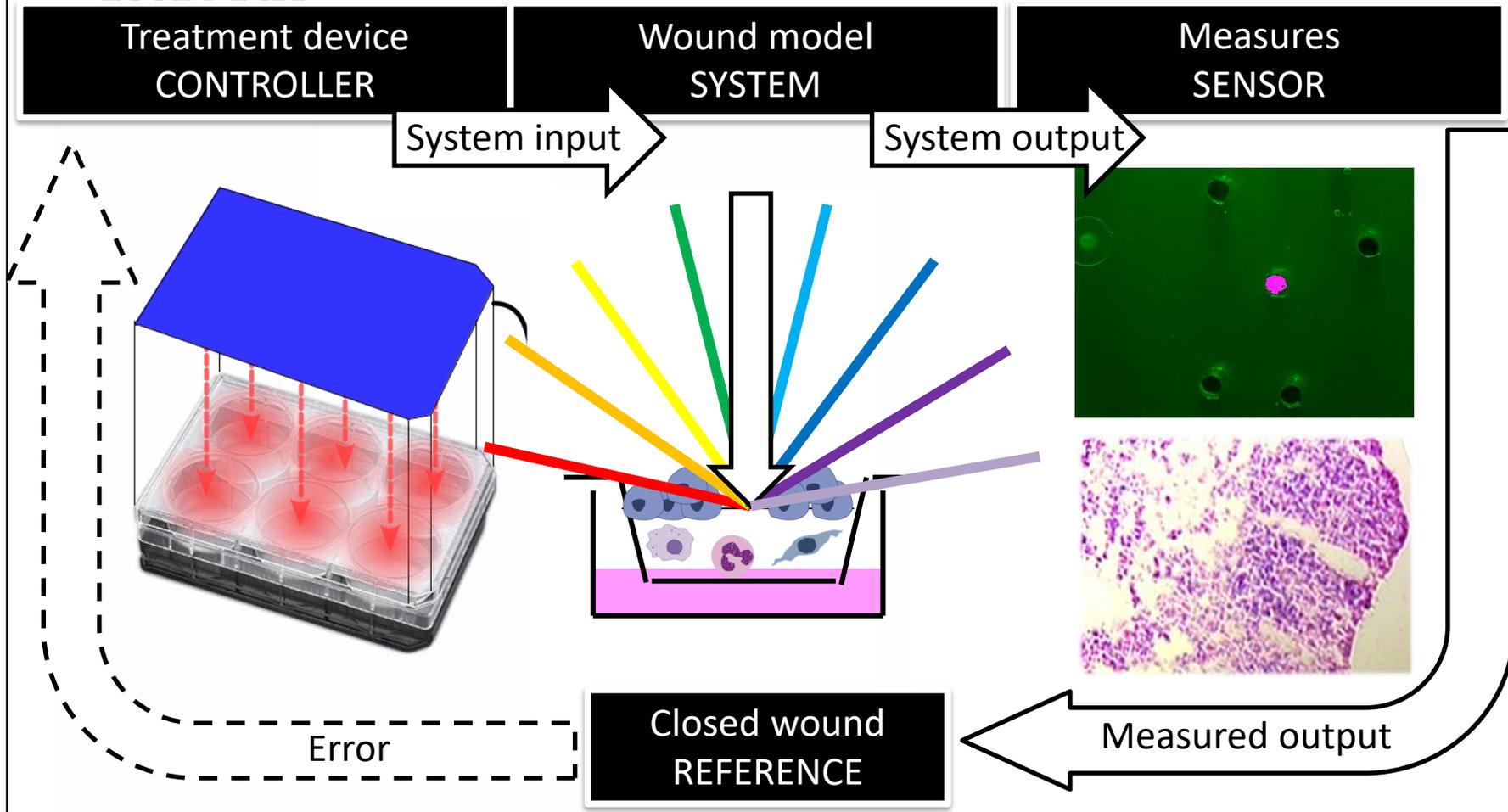
3) Exposure Time

16% no ,protocol'

Advanced wound care

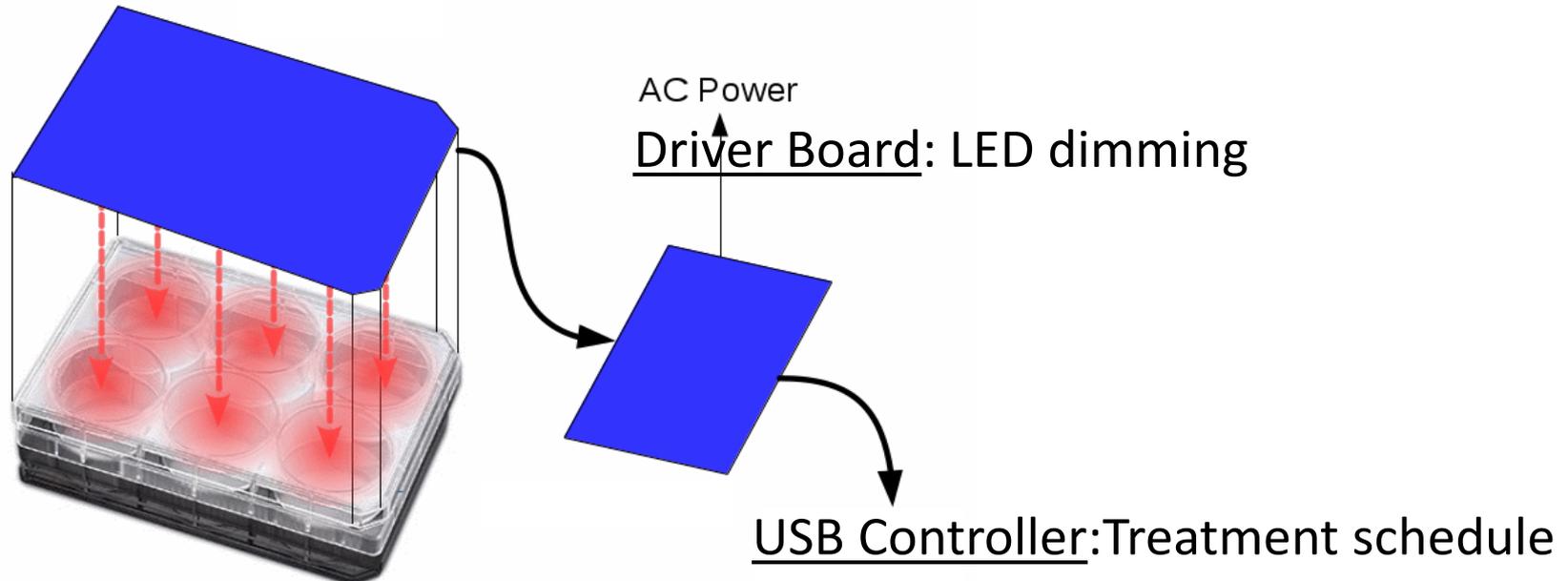
- Optimal treatment parameters: **unknown**
- Standard protocols: **none**
- Combinations (light + mechanical + electrical): **none**

APPROACH: Modeling + control of the wound



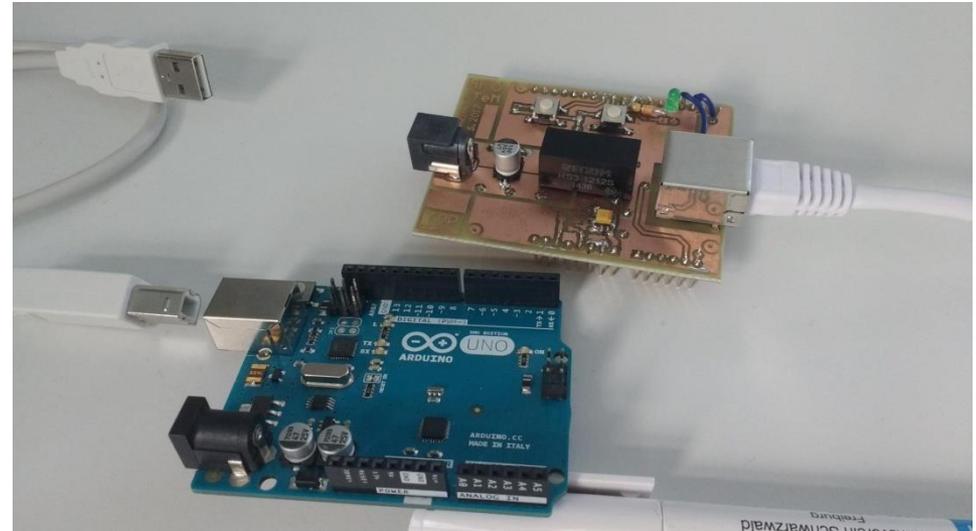
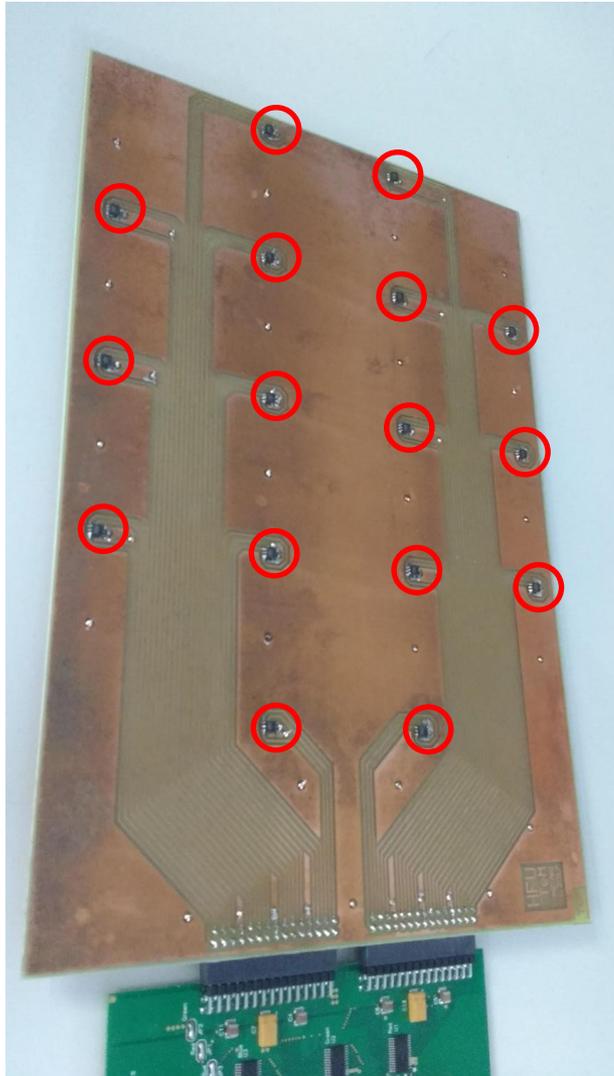
Prototype device: adjustable treatment parameters for automated and repeatable in vitro experiments.

LED Board: Independent control of LED



- Prescribed parameters: Wavelength, Irradiance, Time
- Performance: Uniform treatment delivery to target surface
- Prototype: 2x2 RGB LED array (Results presented)

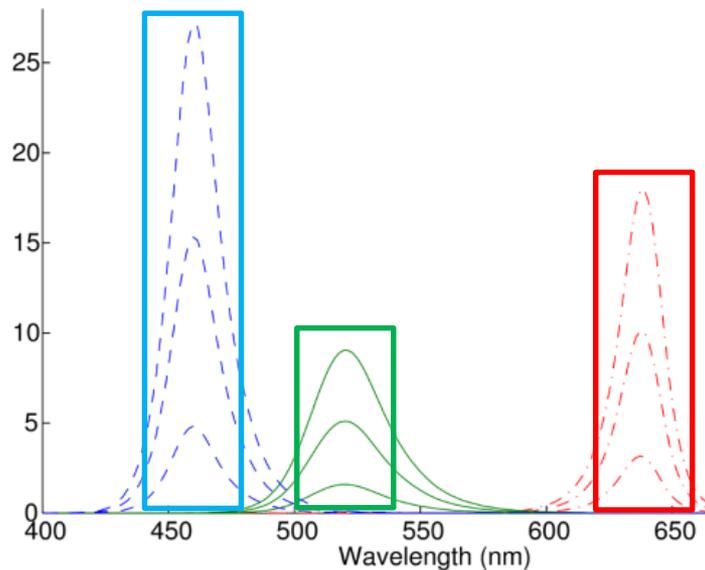
Prototype: Updated LED board and Arduino controller



- RGB LED wavelengths
- Uniform irradiance
- Programmable schedules
- Functional in incubator !!!

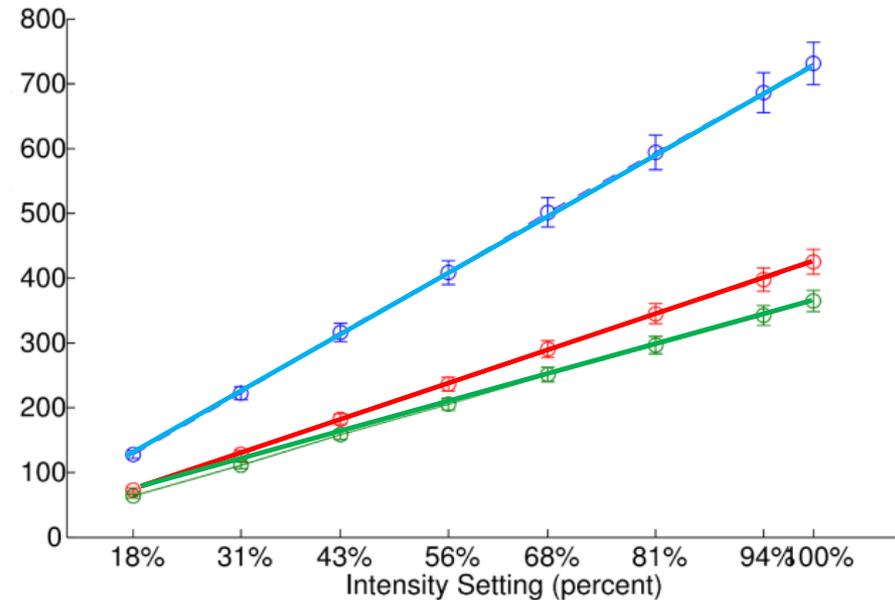
Irradiance measures [mW/m²] at intensity settings.

1) Spectral irradiance



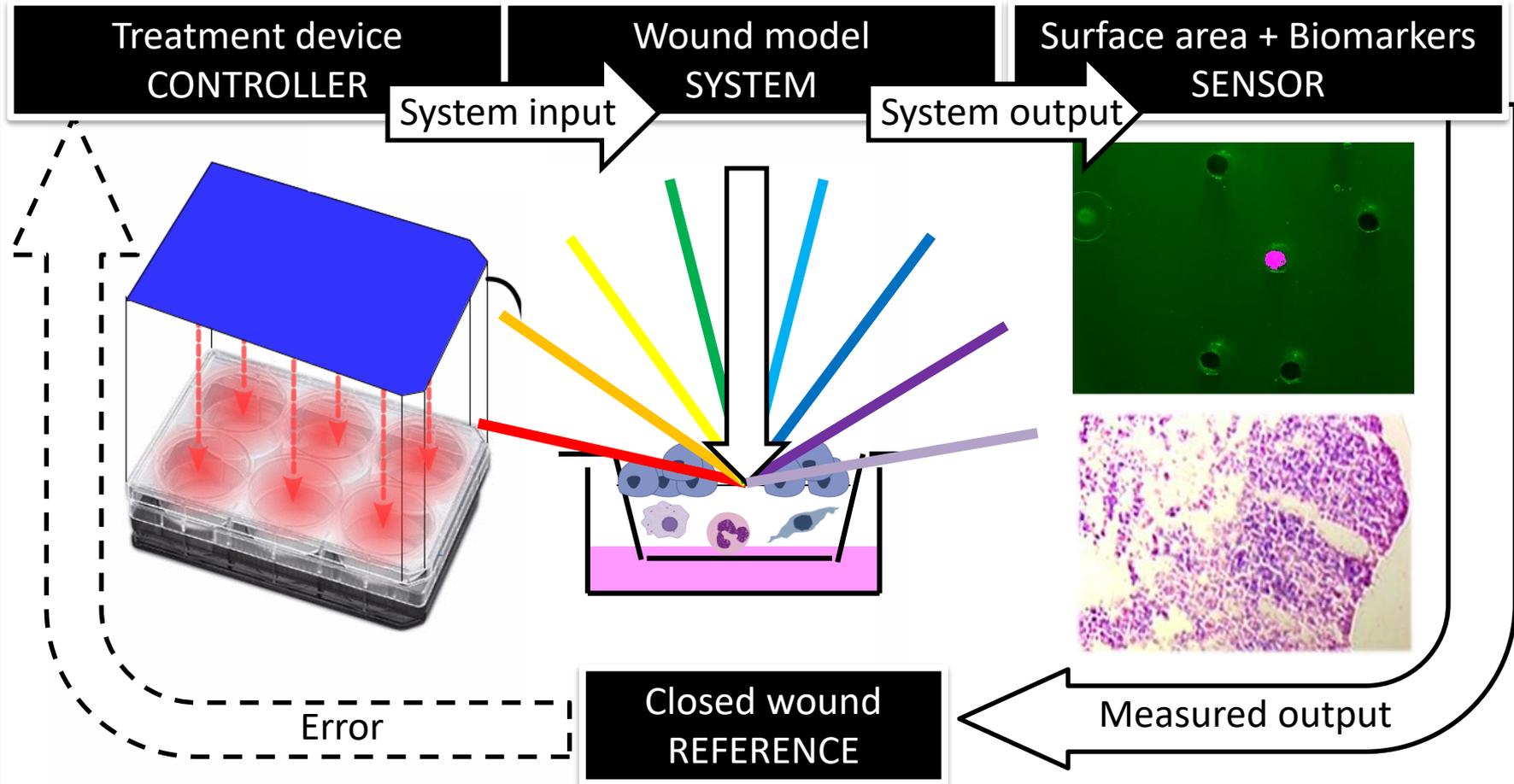
LED dimming (PWM method) does not alter wavelength.

2) Integrated irradiance



Measurements determine device emission, but not tissue absorption....

Ongoing studies to establish dose-response relationships to guide wound healing therapy



**Thank you for
your attention**