

The Future Is Now - EPID In Vivo Dosimetry

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Symposium 2020

UC San Diego
RETHINKING MEDICAL PHYSICS



Disclosures

- Receive grant funding from Varian Medical Systems

Outline

- **Errors detected by pre-treatment vs in-vivo measurements**
 - For ideal detection scenarios and real life practice
- **Methods to analyze in-vivo EPID data**
 - Forward projection image predictions
 - Back-projection dose estimates
- **Current clinical implementation and experience gained from in-vivo use to date**
- **How automation aids implementation. Commercial software available**
- **Requirements for widespread implementations**
 - Complementary QA checks needed
- **Future clinical uses**
 - Real-time error detection
 - Uses in adaptive planning

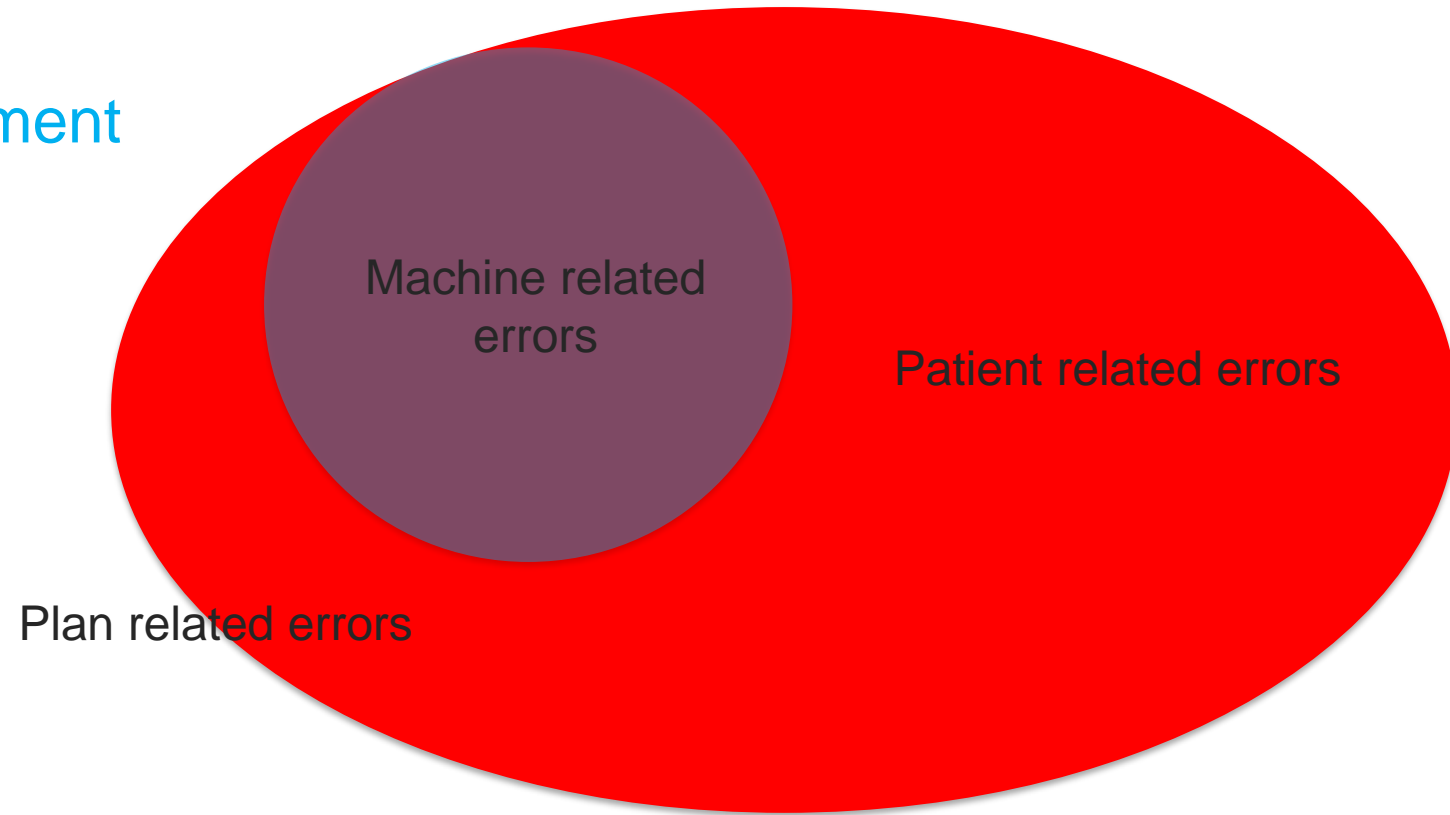
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Error Detection with the EPID

Pretreatment

In-vivo



Potential Error	Error Type	References
Machine-related	Transfer error	Mans et al. (2010), Mijnheer et al. (2015)
Plan-related	Dose calculation error	Mans et al. (2010), Fidanzio et al. (2015), Mijnheer et al. (2015)
	Immobilization system not included in the treatment plan	Fidanzio et al. (2015)
	Bolus material not taken into account	Mijnheer et al. (2015)
Patient-related: anatomy changes	Changes in atelectasis and pleural effusion	Piermattei et al. (2009), Mans et al. (2010), Persoon et al. (2012), Wendling et al. (2012), Persoon et al. (2013), Fidanzio et al. (2015), Mijnheer et al. (2015)
	Variation in patient contour when the patient becomes more relaxed during treatment	Mans et al. (2010), Fidanzio et al. (2015), Peca et al. (2015)
	Gas pockets in the planning CT scan resulting in an underdose in the PTV during treatment	Camilleri et al. (2014), Cilla et al. (2014), Fidanzio et al. (2015)
	Weight loss resulting in an overdose in the PTV during treatment	Mans et al. (2010), Camilleri et al. (2014), Cilla et al. (2014, 2016)
	Incomplete bladder filling resulting in an overdose in the PTV during treatment	Ricketts et al. (2016)

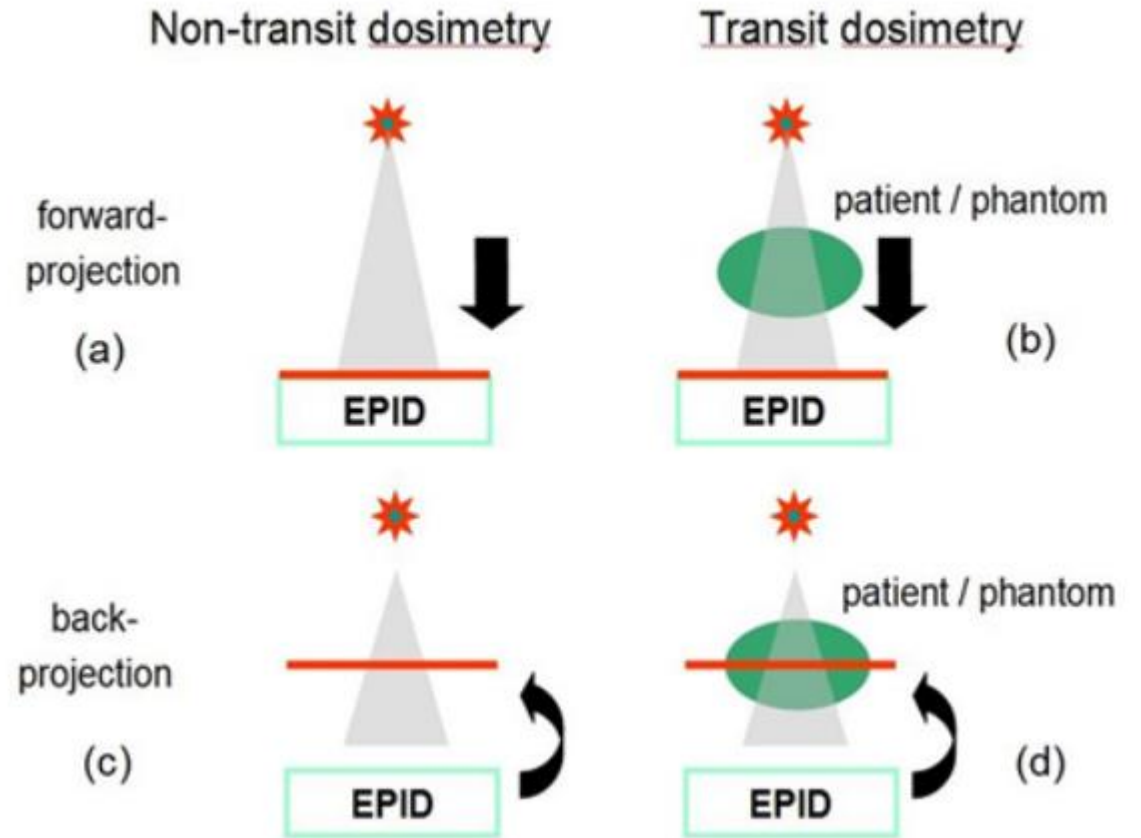
Potential Error	Error Type	References
Patient-related: delivery errors	Bar of the treatment couch in the entrance beam during treatment	Piermattei et al. (2009), Fidanzio et al. (2015)
	Imperfect immobilization allowing the patient to move during treatment	Hanson et al. (2014), Cilla et al. (2016)
	Wrong patient setup during treatment	Fidanzio et al. (2015), Mijnheer et al. (2015)

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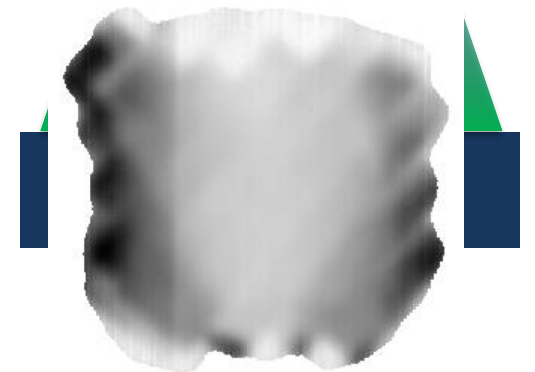
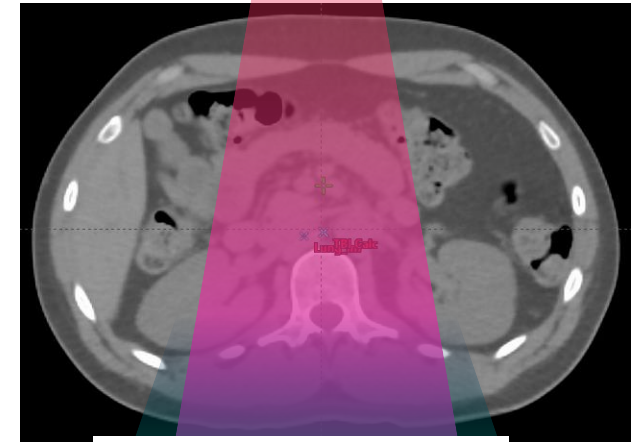
Measurement Approaches

- **Non transit dosimetry**
 - Make a prediction of EPID image no patient/phantom in the way.
 - From EPID image make a prediction of the fluence at isocenter.
- **Transit Dosimetry**
 - Make a prediction of the image.
 - From the image make a prediction of the dose.



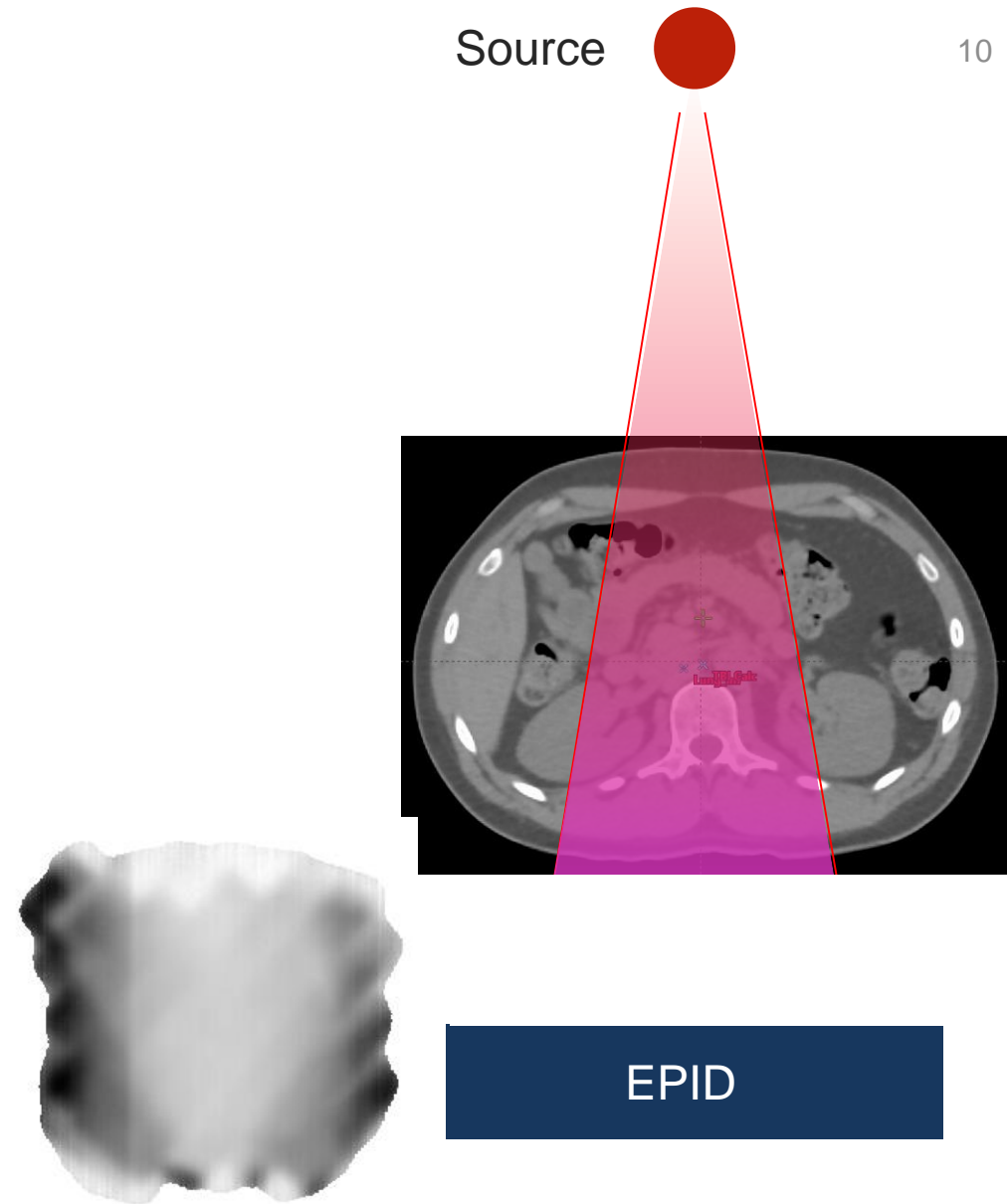
Transit Dosimetry (forward projection)

- Determination of greyscale image at the level of the EPID
 - Primary Fluence
 - Scattered Fluence
 - Response of the EPID



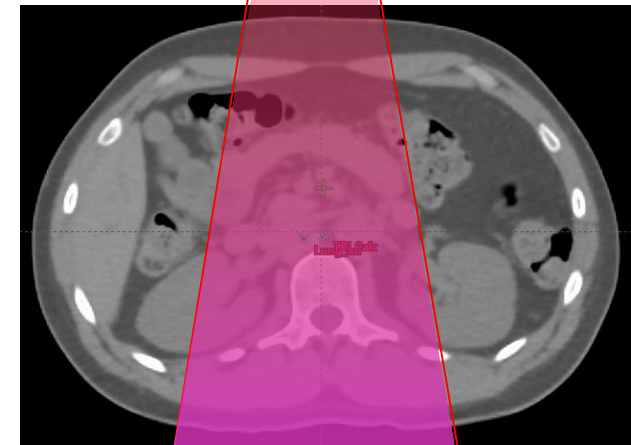
Back Projection (3D)

- Reconstruct dose in patient
 - From EPID image estimate primary fluence and scattered fluence at EPID level
 - Separate primary fluence
 - Back-project primary fluence to incident fluence
 - Use incident fluence to estimate dose



Back Projection (3D)

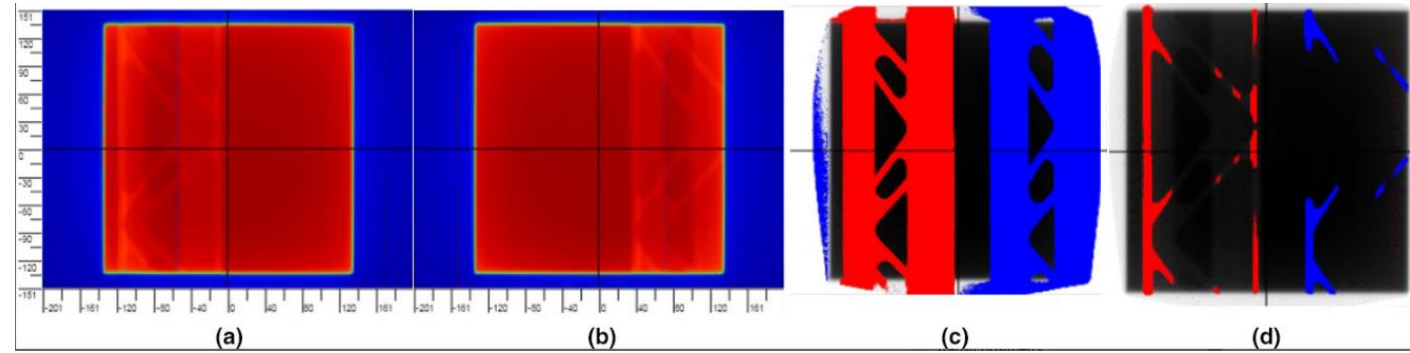
- EPID image is measured with patients anatomy during treatment.
- However dose is calculated on anatomy acquired during planning.
- Able to detect changes in planned dose.
- Does not calculate delivered dose!
- Need CBCT.



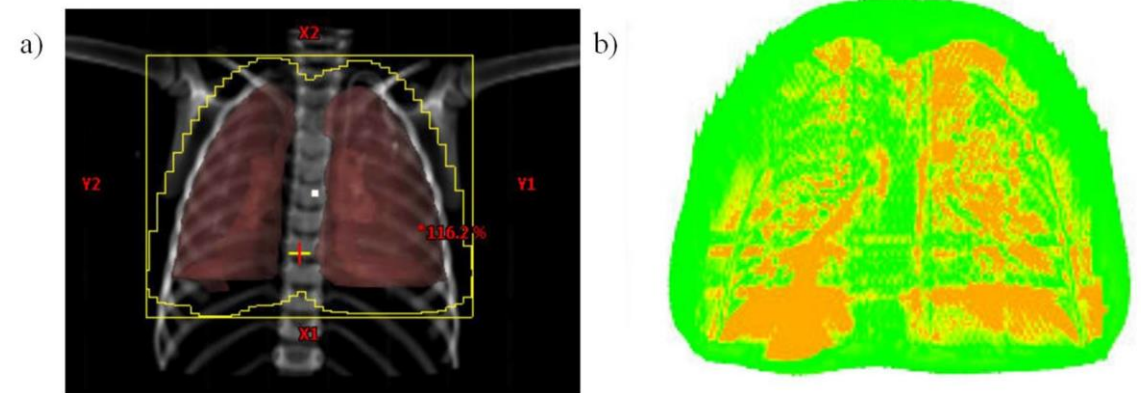
EPID

Image Difference

- Compare EPID images day 1 to EPID image day n
- Relative differences



Zhuang, Olch. J Appl Clin Med Phys 2018



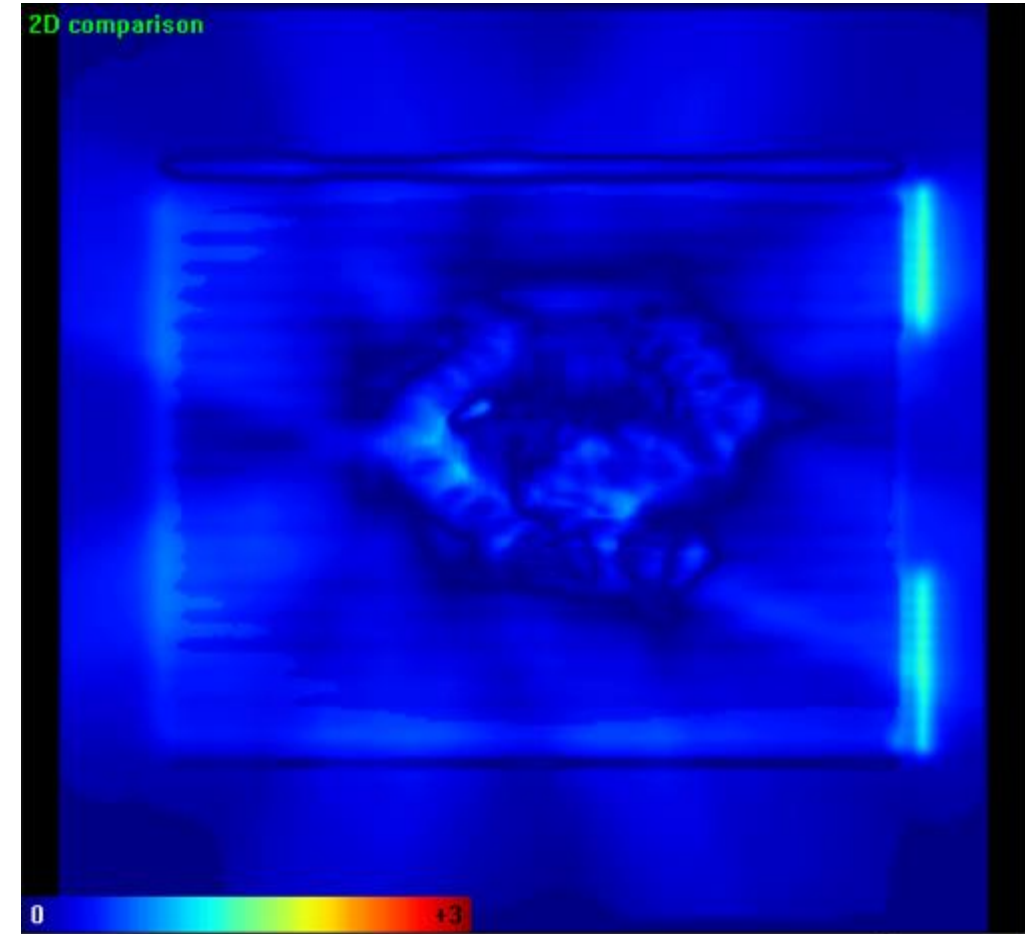
Olch et al

Adv. In Rac Onc 2019

Planar Gamma Evaluation

Comparisons

- Image level
 - 0D point comparison
 - 2D image comparison
- Patient level
 - 0D point comparison (isocenter)
 - 2D plane comparison
 - 3D volumetric comparison
- Typically Gamma Comparison



Pros and Cons

Method	Pros	Cons
Point Dose	<ul style="list-style-type: none">• Simple quick algorithms• Simple to commission	<ul style="list-style-type: none">• Sensitivity to errors reduced• Less information available
3D Dose	<ul style="list-style-type: none">• 3D dose map• Able to reconstruct DVHs	<ul style="list-style-type: none">• More complex to commission

Analysis

Patient Name **Hansen, RT SKULL 3**
 Fraction Number **27**

Plan Name **KSH_7F_IMRT1**
 Date Delivered **13 Jul 2015**

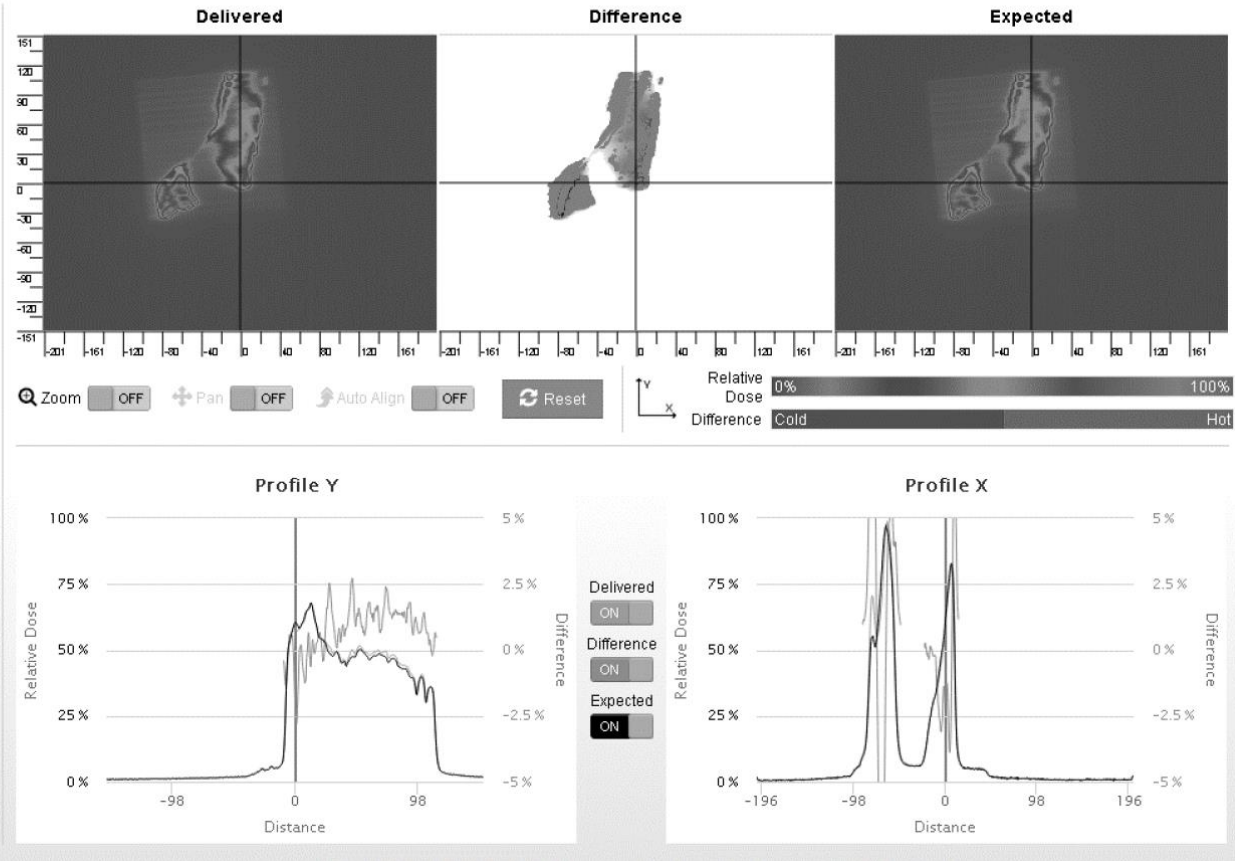
Average Passing Rate **57.41% (Failed)**
 Machine Name **TrueBeamSN1572**

Beams	
✓ 0	99.77 %
! 51	48.72 %
! 102	32.96 %
! 153	62.76 %
! 204	67.41 %
! 255	40.02 %
! 306	46.74 %

Analysis Settings	
Method	Difference
TH (%)	10
Normalization	Global
DIST (mm)	N/A
Low Grad (%/mm)	N/A
DIFF (%)	1
High Grad (%/mm)	N/A
Baseline	Fraction 17 (13 Jul 2015)

▶ Calculate

Results	
Passing % (points)	33 (17,258)
Failed High % (points)	53 (27,749)
Failed Low % (points)	14 (7,350)
Total Points	52,357
Average (Standard Deviation)	1.82 (3.79)



Hsieh et al. Prac Rad Onc, 2017,

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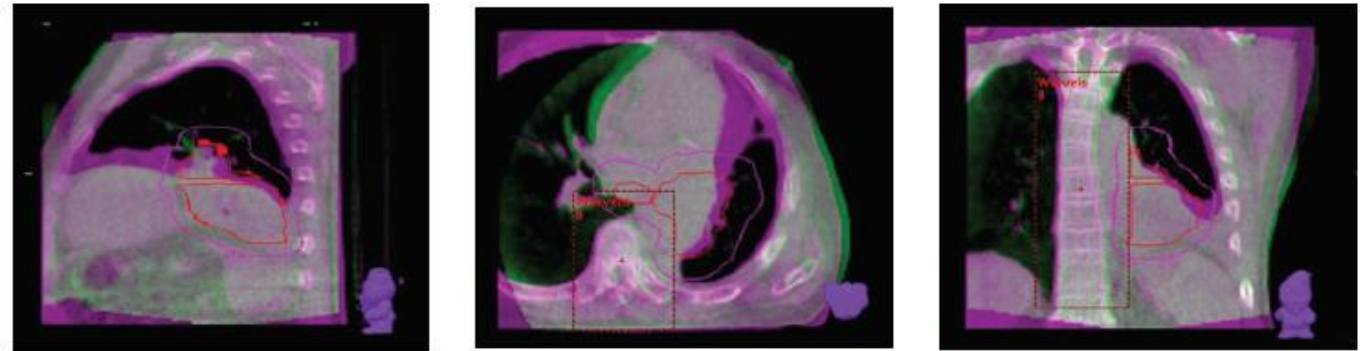
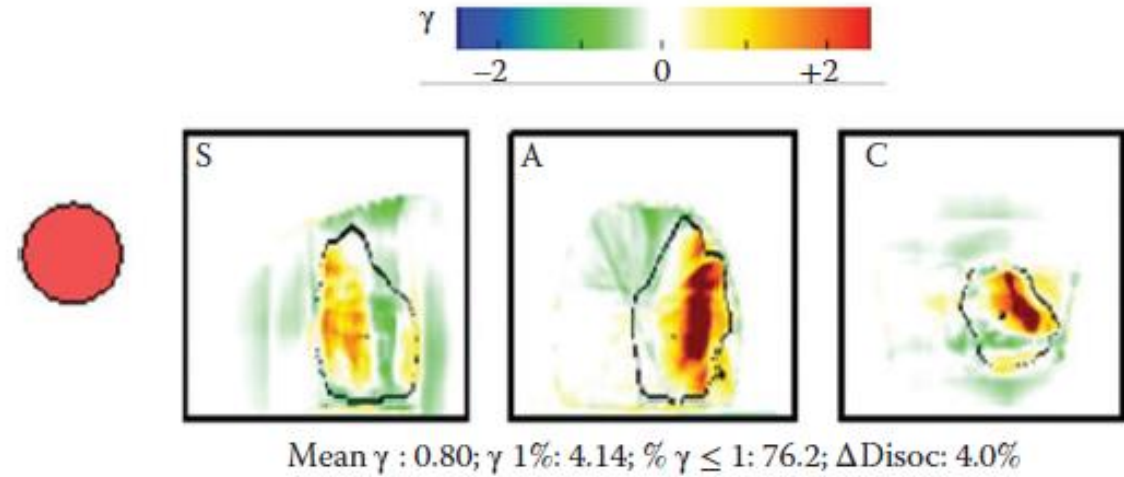
In the Clinic

- NKI has been using in-vivo system clinically for a long time.
 - Have replaced pre-treatment with in vivo measurements.
 - Detected 17 major errors 2005-2009 (over 4000 patients)
 - 9 of these errors would have been missed with Pre-treatment only

TYPE OF ERROR	NUMBER OF ERRORS
PATIENT ANATOMY	7
ACCIDENTAL PLAN MOD	2
PLAN TRANSFER	4
SUBOPTIMALLY TUNED TPS	2
FAILED DELIVERY	2
DOSIMETRICALLY UNDELIVERABLE PLAN	1
TOTAL	17

Lung

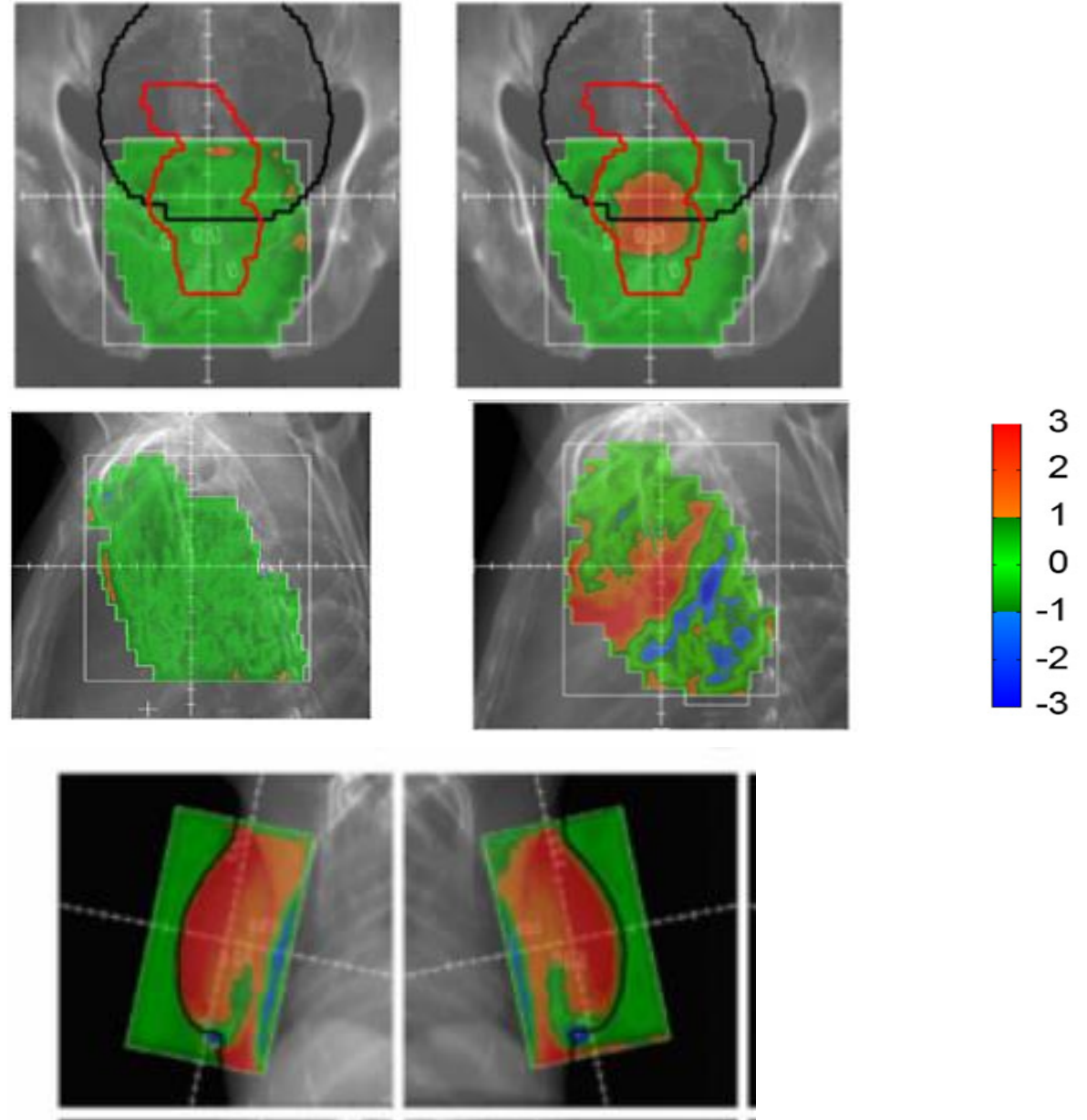
- Alert raised by EPID measurement
- Comparison of CBCT (green) and planning CT (purple)
- Reduction of Atelectasis
- Replanning scan was made



Clinical 3D dosimetry in Advanced Radiotherapy. Mijnheer

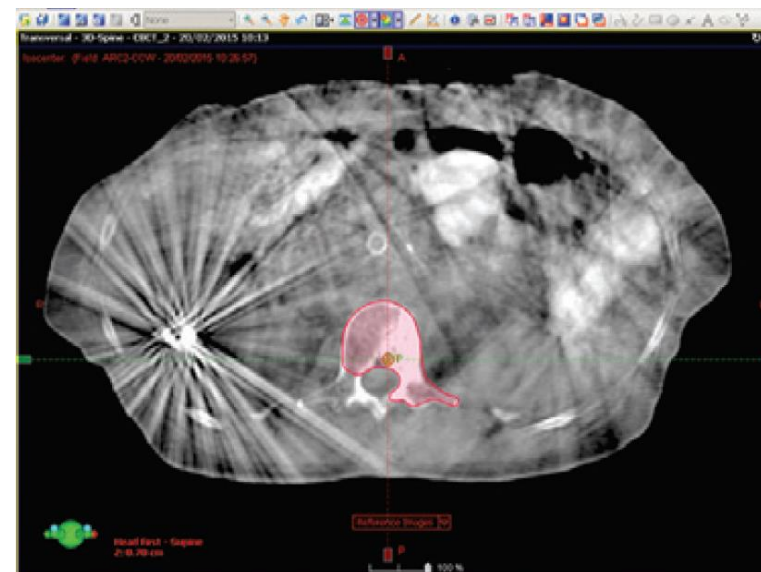
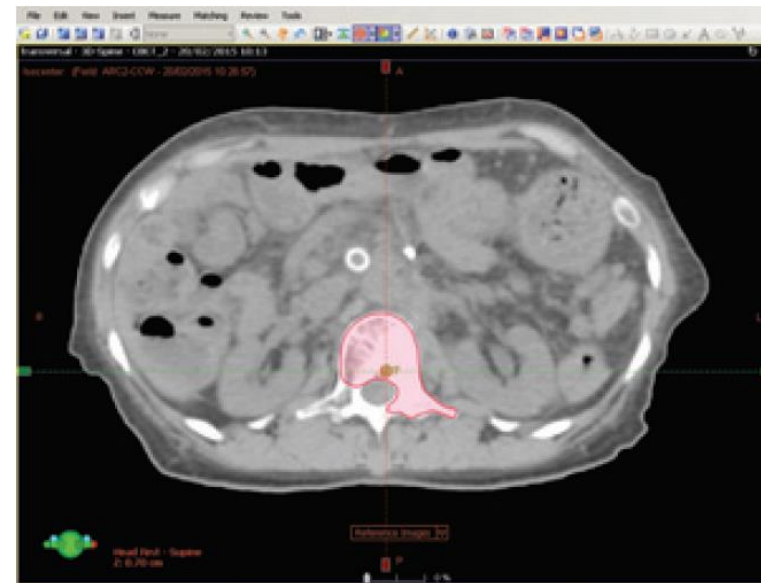
Prostate, Lung, Breast

- Gas bubbles
- Change in atelectasis
- Setup for breast patient



Spine

- 25% decrease in 3D gamma pass rate
- Stent moved into treatment field between fractions

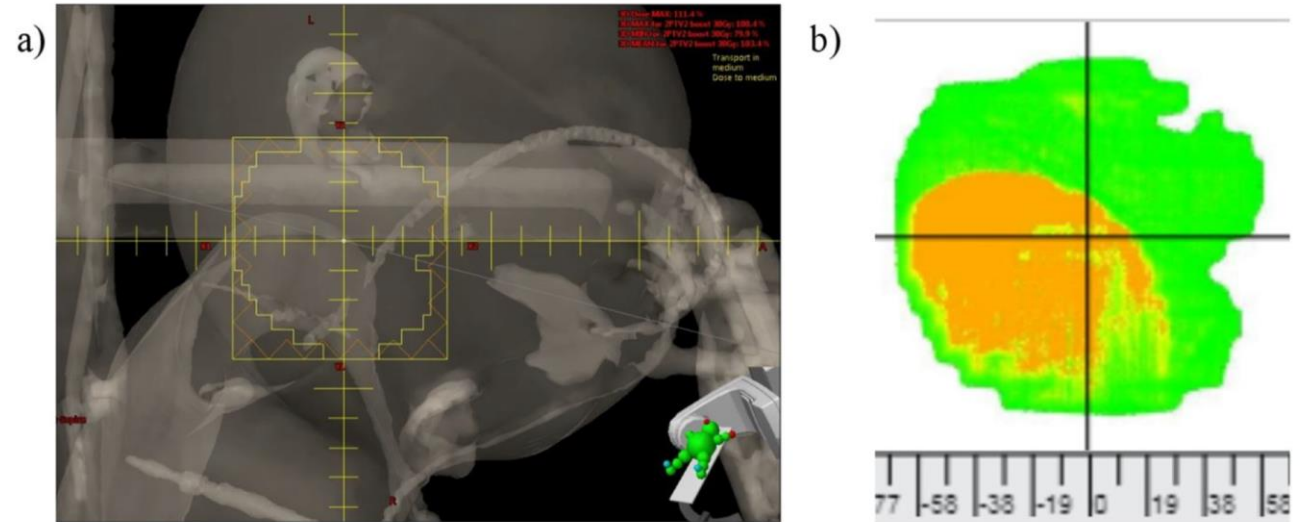


Van Uytven et al. Med Phys 2015

Clinical 3D dosimetry in Advanced Radiotherapy. Mijnheer

Shoulder

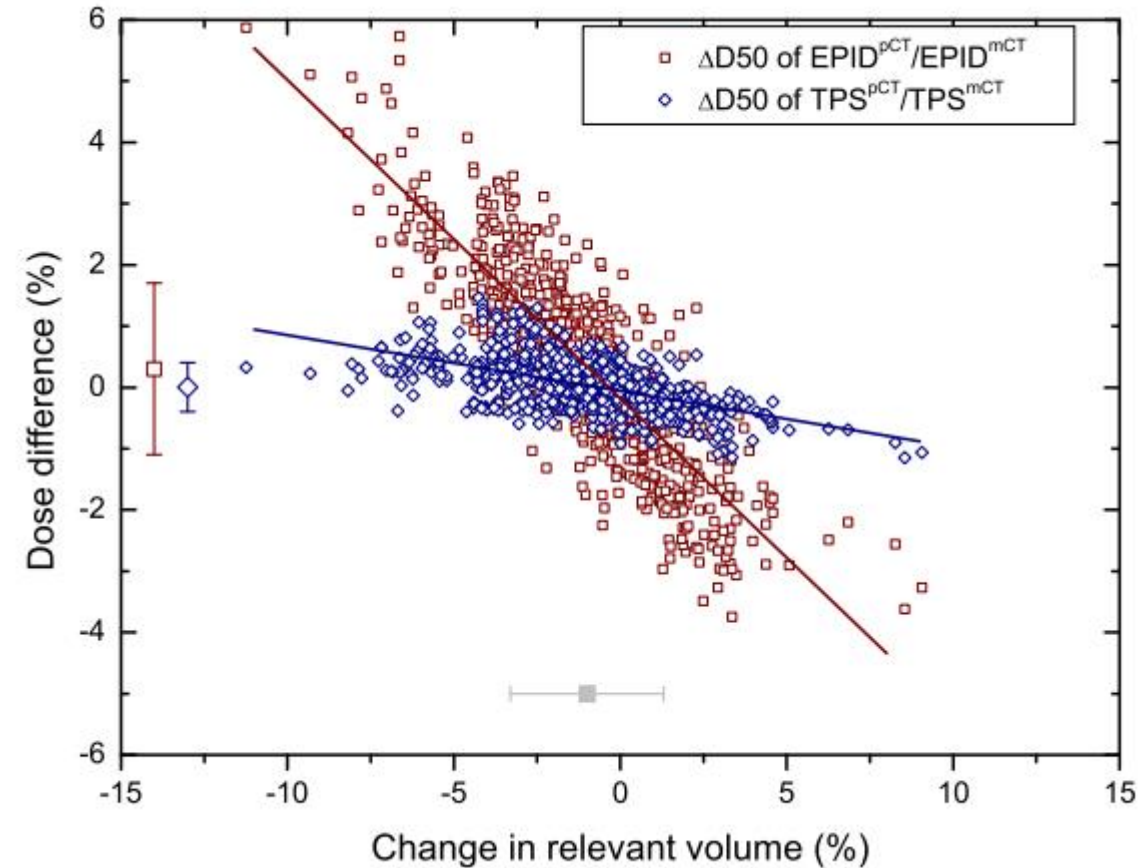
- Image comparison with first fraction shows change in shoulder position



Olch et al. Adv. In Rac Onc 2019

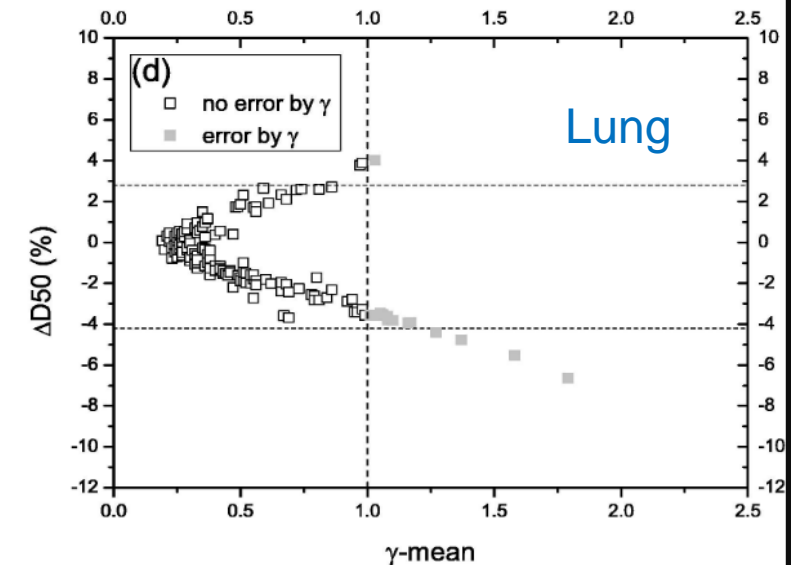
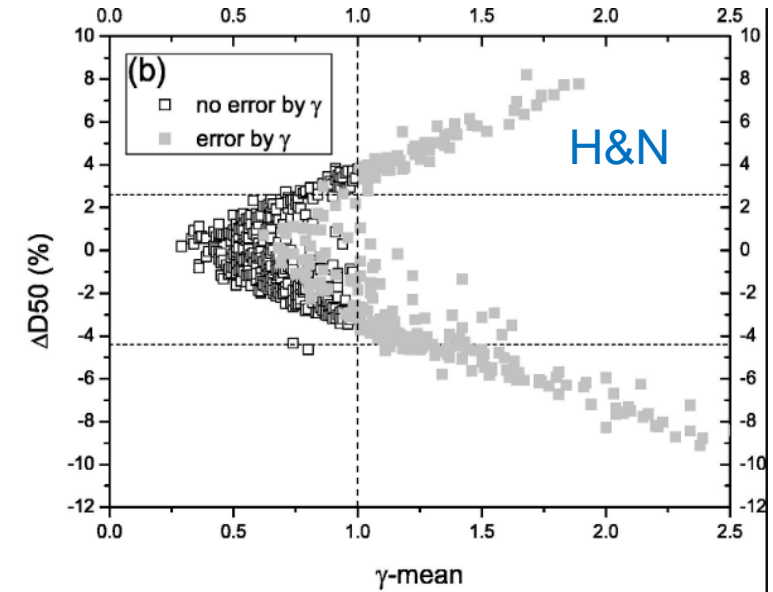
Clinical Impact of Errors

- Head and Neck treatments
- Planning CT deformed to CBCT
- Change in EPID dose and TPS dose for $\Delta D50$
- EPID has enhanced sensitivity



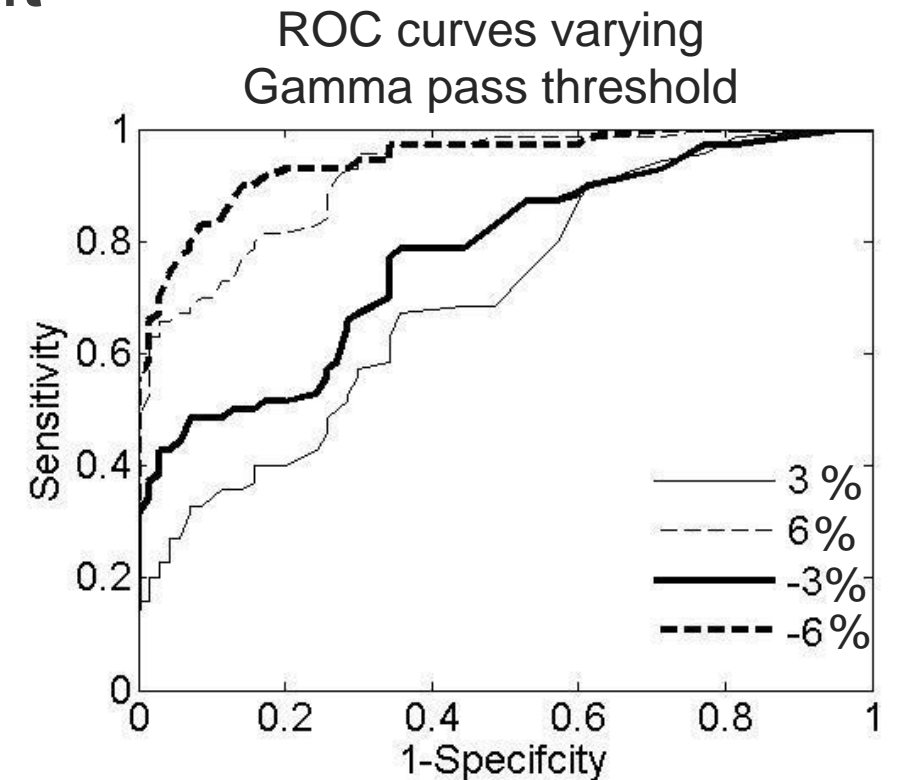
Clinical Impact of Errors

- Tolerance levels on mean gamma and gamma 1%.
- Compare gamma mean and $\Delta D50$ for H&N and Lung
- Good correlation for lung less specific for H&N.



Setting Tolerance Levels

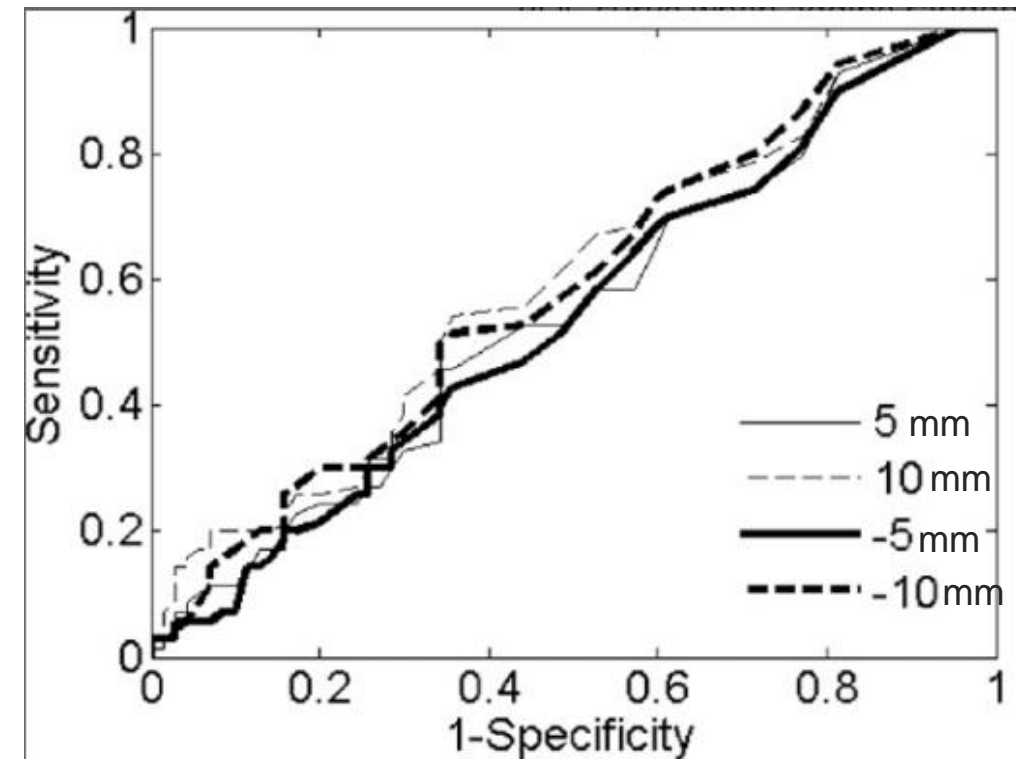
- Model EPIDs sensitivity to different errors
 - Deliver plan, introduce errors in TPS
 - Measures changes in gamma pass rate(3%/3mm)
 - Construct ROC
 - Investigate changes in PTV dose metrics



Setting Tolerance Levels

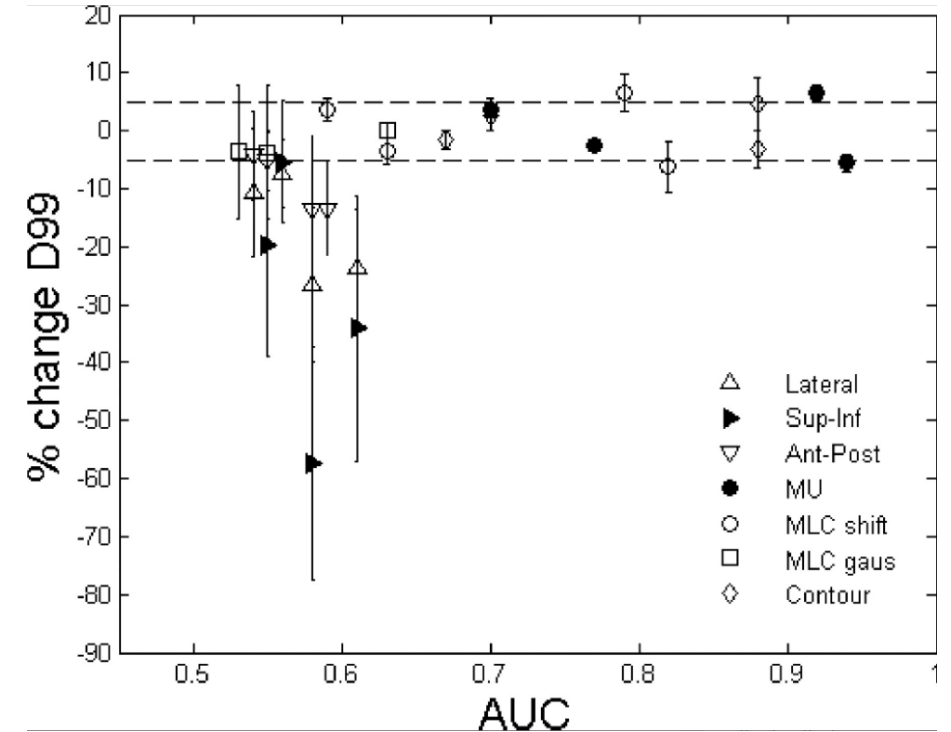
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ROC curves varying
Gamma pass threshold



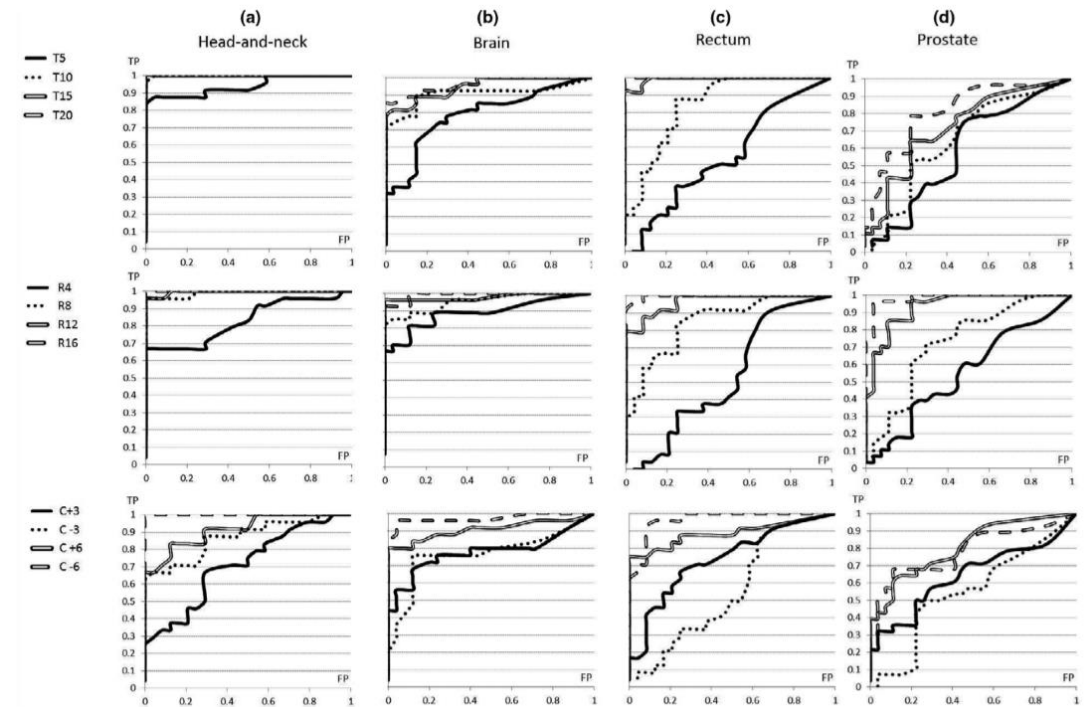
Clinical Impact of Errors

- ROC analysis, compare AUC vs change in D99.
- Different errors introduced
 - MU scaling
 - MLC shifts
 - Patient contour changes
 - Patient shifts



Clinical Impact of Errors

- Simulated errors in synthetic CT.
- Use various indicators
 - ΔDiso , $\gamma\text{-mean}$, $\gamma\text{-max}$, $\gamma\text{-passrate}$, ΔPTV_{D2} , ΔPTV_{D50} , ΔPTV_{D98}
- Use different in vivo alert criteria per treatment site
- Excellent detection of transitions, rotation, contour changes for expect for prostate sites



Challenges to Setting Thresholds

- Different dose calculations
(0D,2D,3D)
- Different algorithms
- Different DVH parameters
(D50, D2,D95)
- Difference treatment sites
- Gamma metrics

Outline

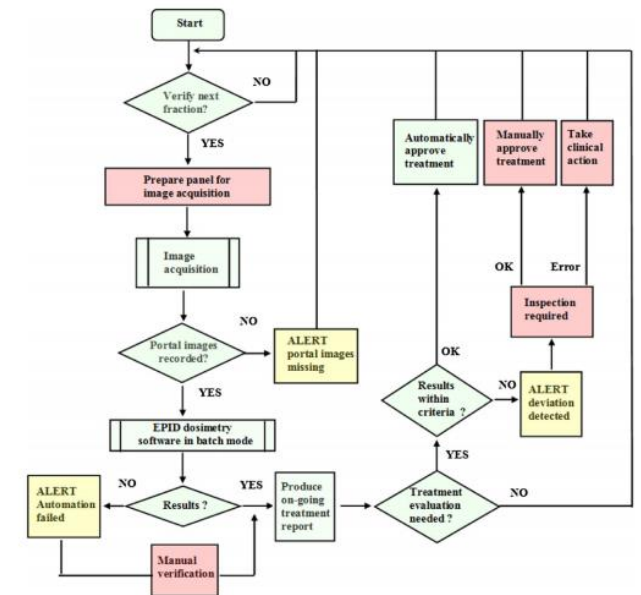
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Automation

- Automation is necessary for implementation, due to the increased workload of additional analysis
- Need to Automate
 - Export (images, other data)
 - Analysis
 - Alerts

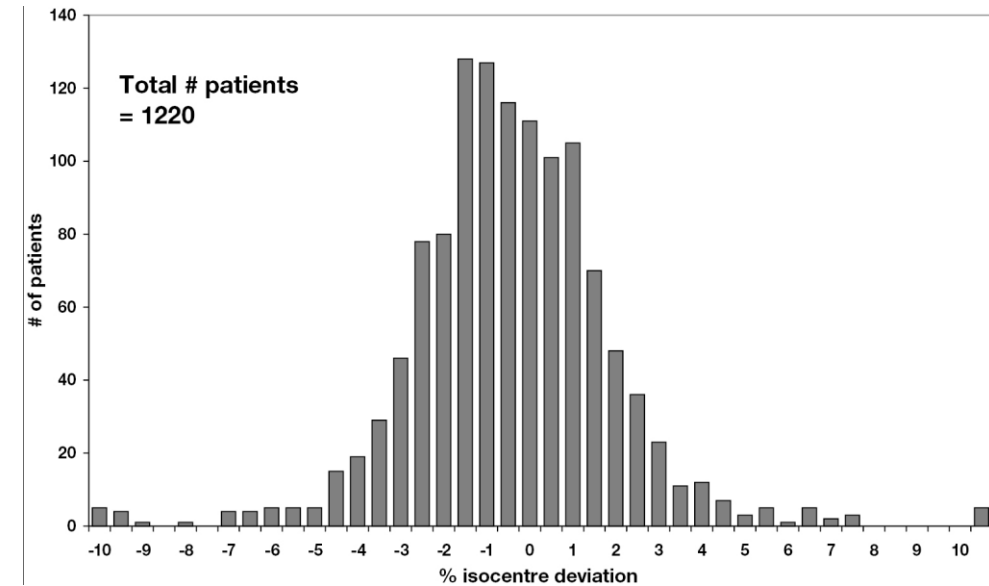
Automation: NKI

- Call verification software after portal images have been recorded
 - Results are available a few minutes after fraction is delivered
Alerts raised if a threshold is exceeded.
 - Significantly reduces workload, less error prone.
 - Alerts grouped into 3 Categories
 - Limitations of calculation model
 - Patient anatomy changes
 - Other (delivery or planning errors, output deviations...)
- Inspection of alerts 0.25 FTE.



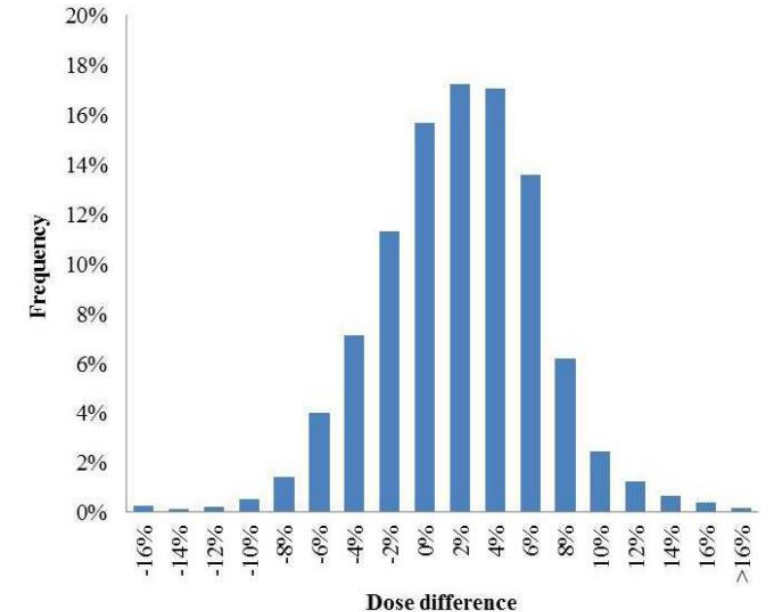
Automation: Royal Marsden

- Based on NKI system
- Compared to TLD measurements less time consuming on unit and analysis. Able to account for deviations based on 2D info
- Replaced nearly all pre-treatment verification
- Flagged when tolerance level is exceeded.



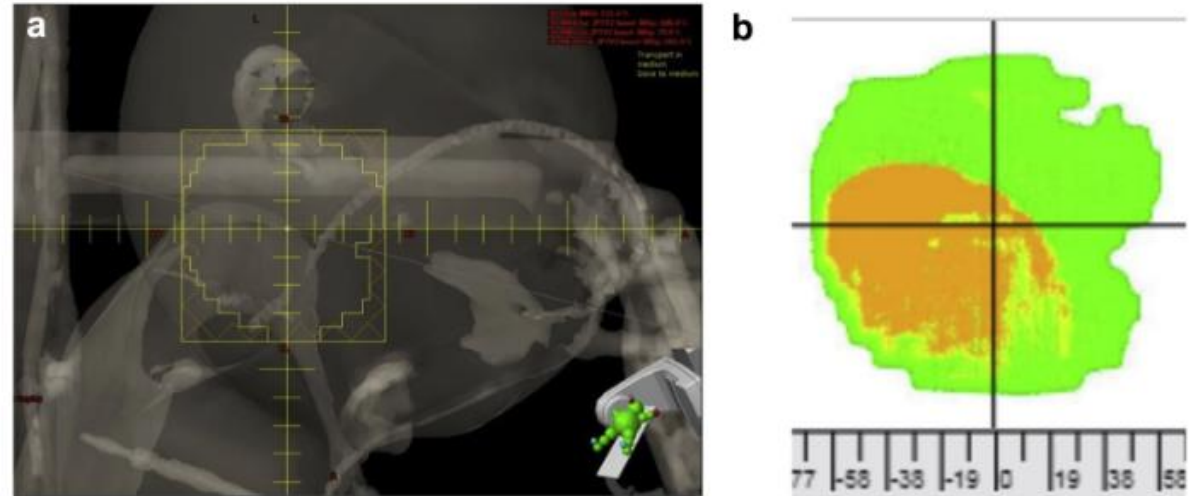
Automation: Institut Curie

- EPIGray
 - Dose to point
- IVD one the first 3 fractions of treatment
- Difference between TPS and dose estimate 1.9% +/- 5.2%
- Automating day to day comparisons



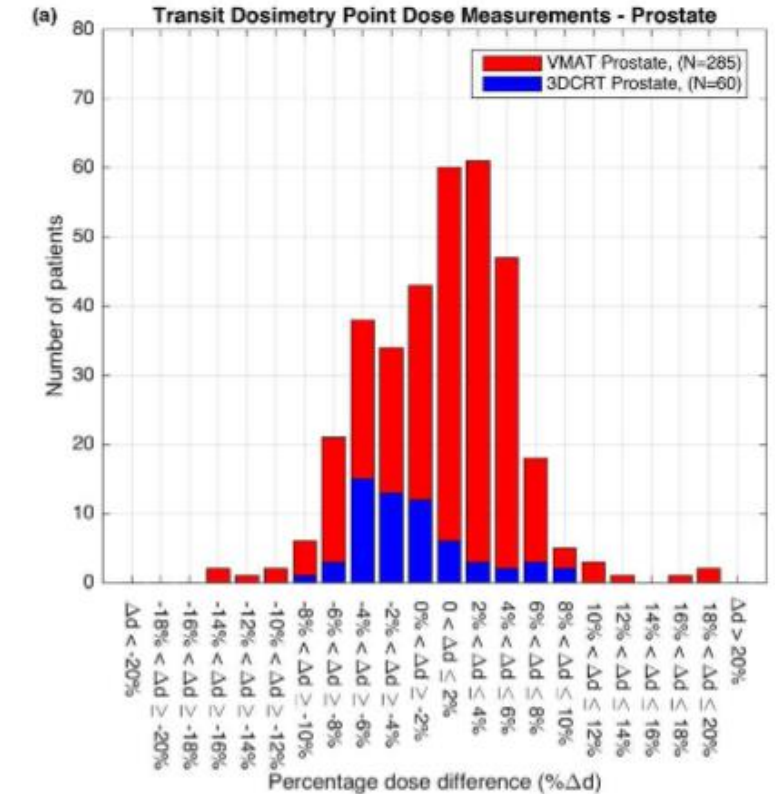
Automation: Children's Hospital Los Angeles

- PerFRACTION
- EPID images compared to baseline images
 - Perform gamma analysis for image, fraction, course of treatment
 - Failures due to body position change, internal anatomy change, external device position, unknown source
- Near total automation



Automation: Edinburgh Cancer Centre

- Dosimetry Check
- Alert triggered when dose difference between TPS and DC at plan ref point exceeds 10%
 - Majority of alerts for breast patients



Commercial Software

- **EPIgray**
 - Celi et al. J Appl Clin Med Phys 2016
- **Dosimetry Check**
 - Gimeno et al. Phys Med 2015,
 - Nailon et al Rad Onc Phys 2019
- **PerFraction**
 - Hsieh et al. Prac Rad Onc, 2017,
 - Zhuang, Olch. J Appl Clin Med Phys 2018,
 - Olch et al. Adv. In Rac Onc 2019
- **SOFTDISO**
 - Cilla et al 2016, Piermattei et al 2018
- **EPIDos**
- **IViewDose**
- **Adaptivo**

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Clinical Implementation

- Selection of system
- Commissioning
- Setting tolerance levels
 - Alert criteria differs from one institution to another
- Follow up actions
 - Policies and procedures for when an alert is raised

Error Types that Still Escape Detection

- **Prescription Errors**

- Error in plans fractionation, location or total dose

- **Incorrect Contouring**

- Portion of contour missing or incorrect volume used for planning

- **Errors in field planning parameters/Suboptimal plan creation**

- Error in field parameters made during planning stage

- **Error detected after fraction is delivered**

- Not suitable for SBRT, SRS treatments

Outline

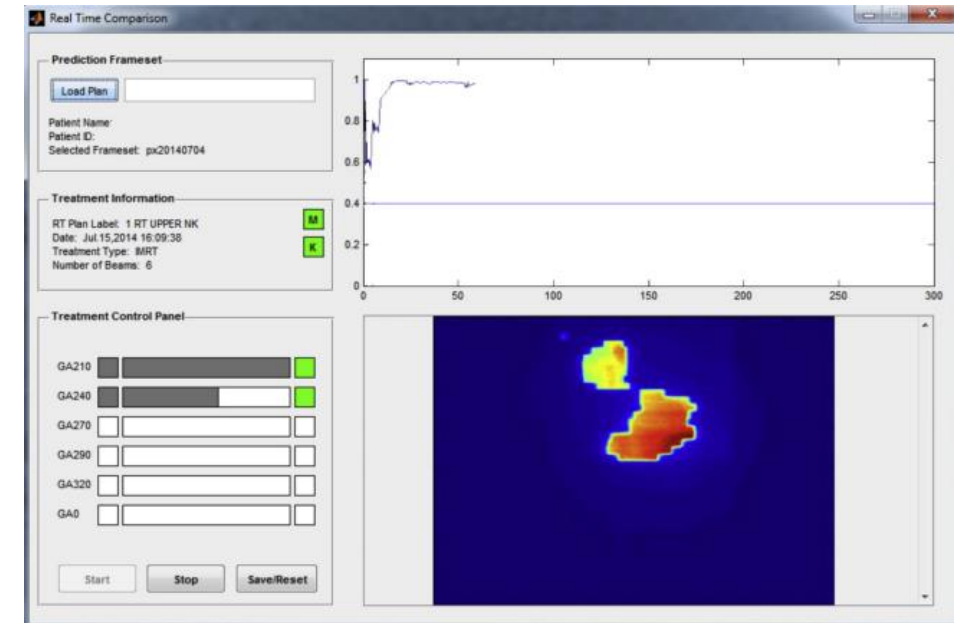
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Real-Time Dosimetry

- Post treatment assessment of some treatments is not clinically useful.
- Diodes/MOSFETS are used to monitor treatments in real time, stop treatment if measured values deviate significantly from planned.

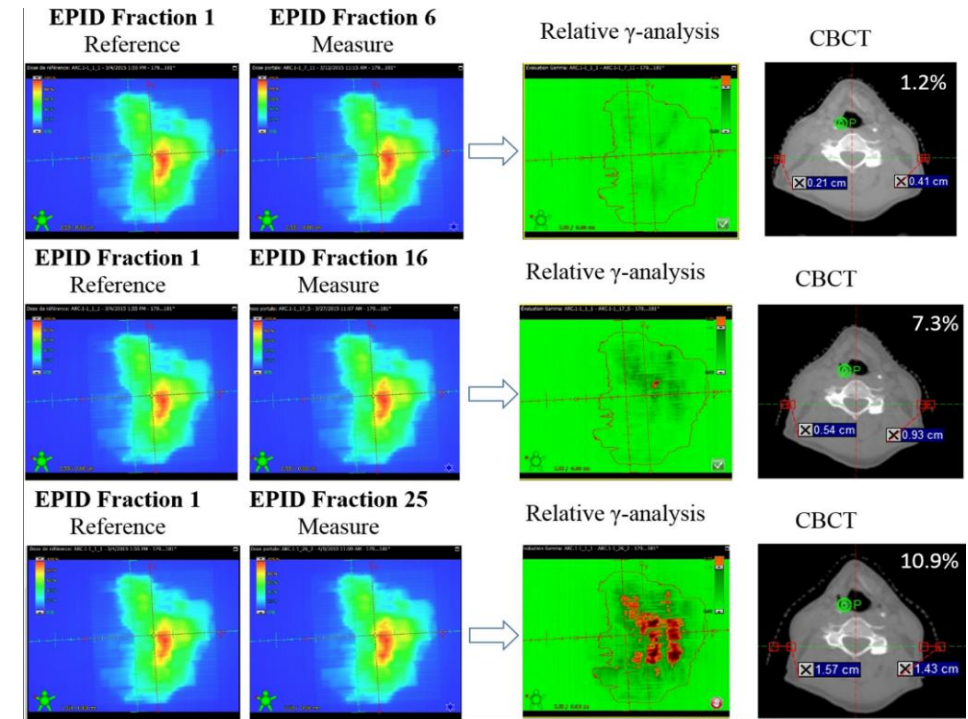
Real-Time Dosimetry

- EPID real-time prediction of images.
- WatchDog Project
 - Reference data set of EPID images is compared to acquired EPID images at a frame rate of 0.1s.
 - Comparison was performed to cumulative frame to gauge overall delivery quality.



Adaptive Planning

- Analysis of lung and head and neck patients have observed progressive anatomical changes
 - In-vivo dosimetry can provide quantitative metrics
- EPID based verification of OAR doses
- Real time adaptation



Concluding Remarks

Additional Resources

- **2016 AAPM Annual Meeting - Session: The EPID Strikes Back.**
 - Peter Greer, PhD
 - <https://www.aapm.org/education/vl/vl.asp?id=11449>
- **Clinical 3D Dosimetry in Modern Radiation Therapy.**
 - In Press, Edited by Ben Mijnheer, PhD

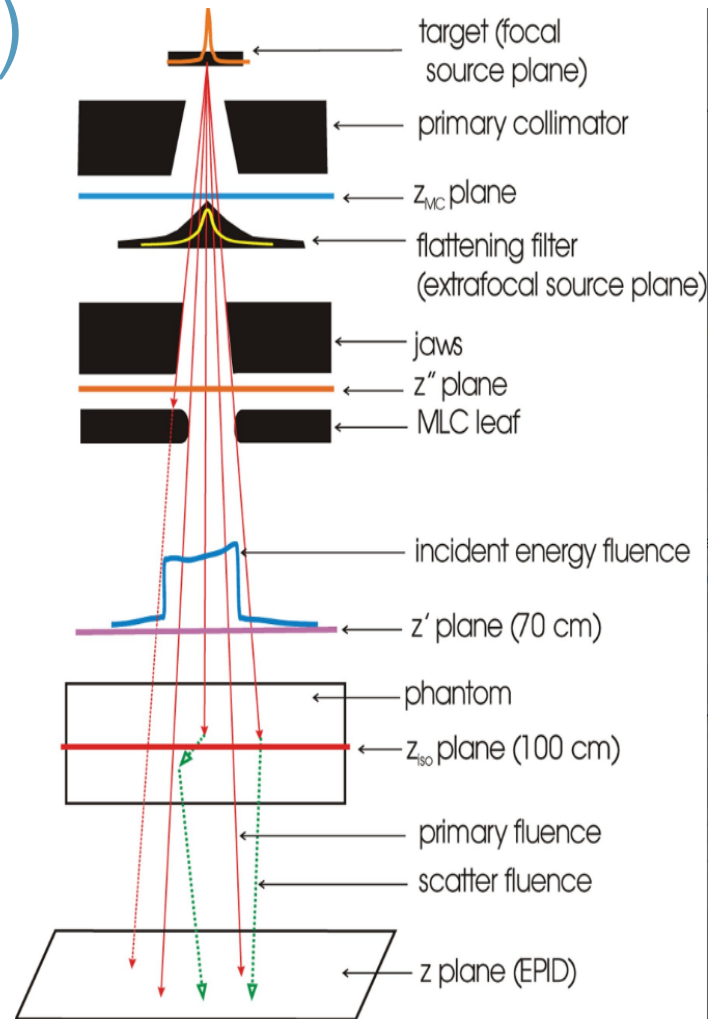


Thank You

Additional Materials

Transit Dosimetry (forward projection)

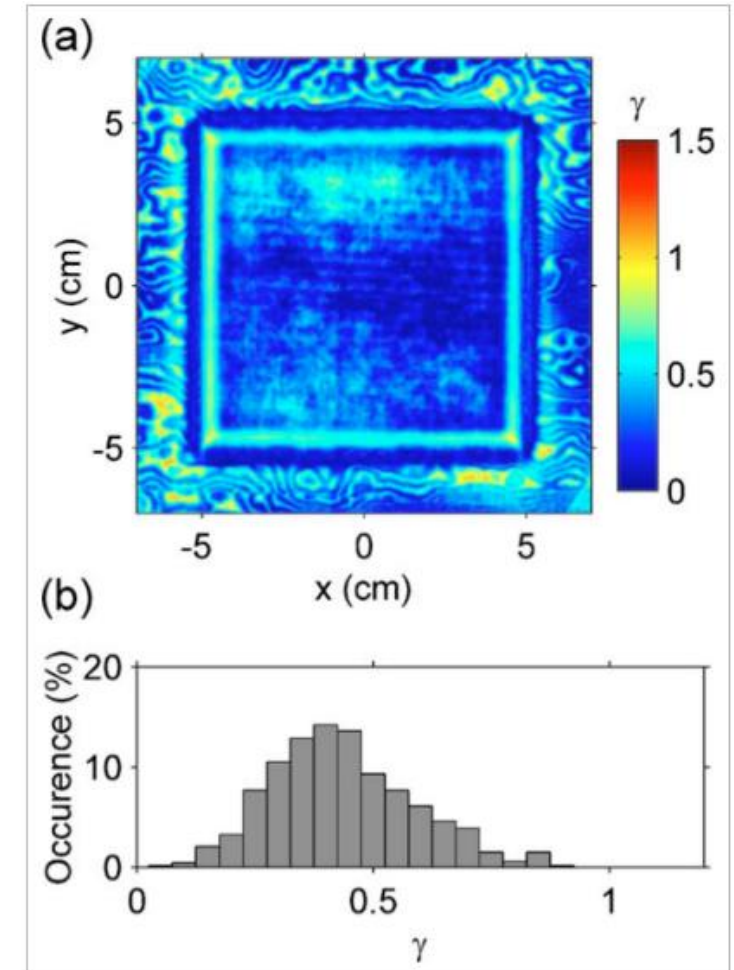
- Use MC methods or empirical calculations.



Chytky et al Med Phys 2013

Back Projection (0D,2D)

- Determination of dose at point in patient (iso)
- Estimation of planar dose
 - Related imager response to radiological thickness of patient/phantom.

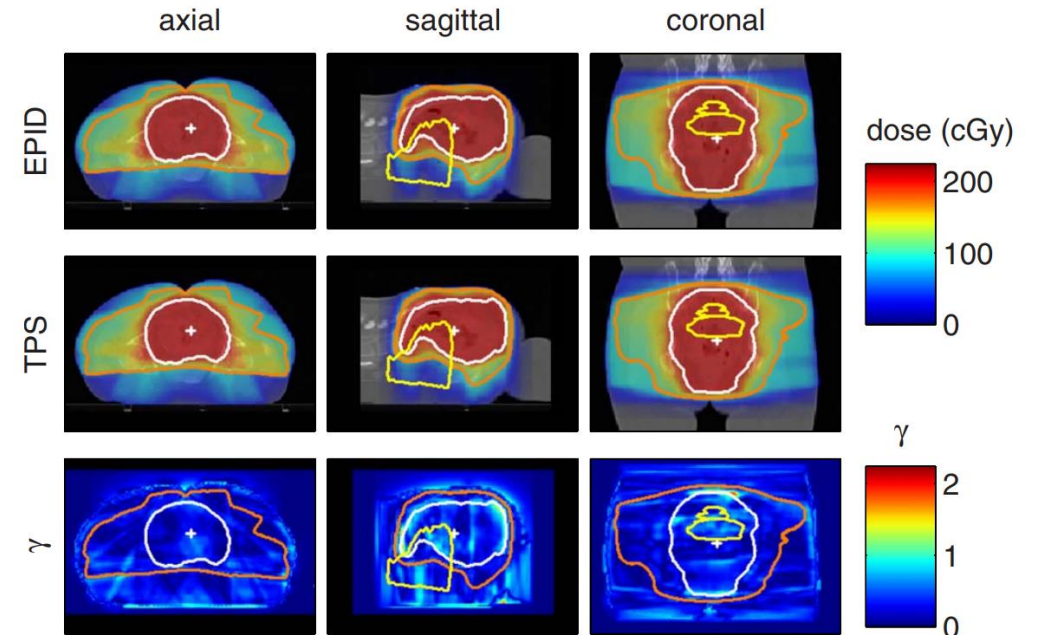


Piermattei et al Med Phys 2008.

Wendling et al Med Phys 2006

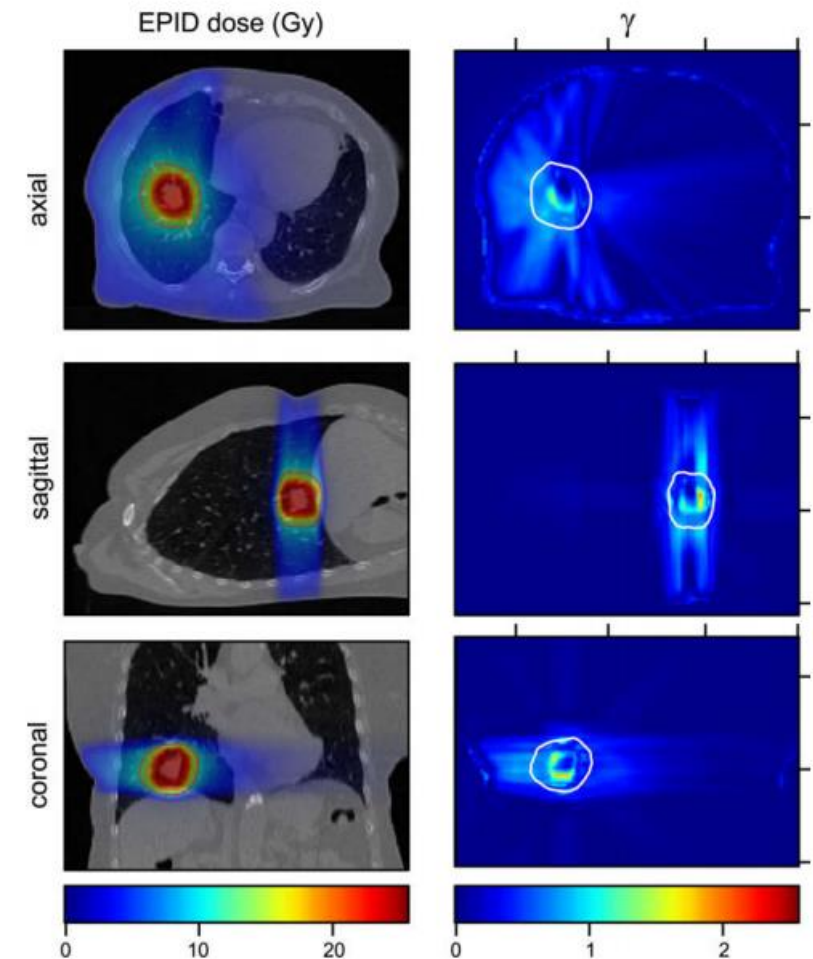
Back Projection (2D-3D)

- Requires collection of open beam image
- Use EPID image to estimate primary and scatter fluence
- Model attenuation of primary fluence through patient CT
- Reconstruction of 2D dose planes, interpolated to reconstruct 3D dose



Back Projection VMAT

- Information is washed out over VMAT Arc
- Use Cine images recording gantry angle to backproject dose at various angles
- Technical challenges
 - Gantry angle lag, missing frames, interplay between pulsing and readout.

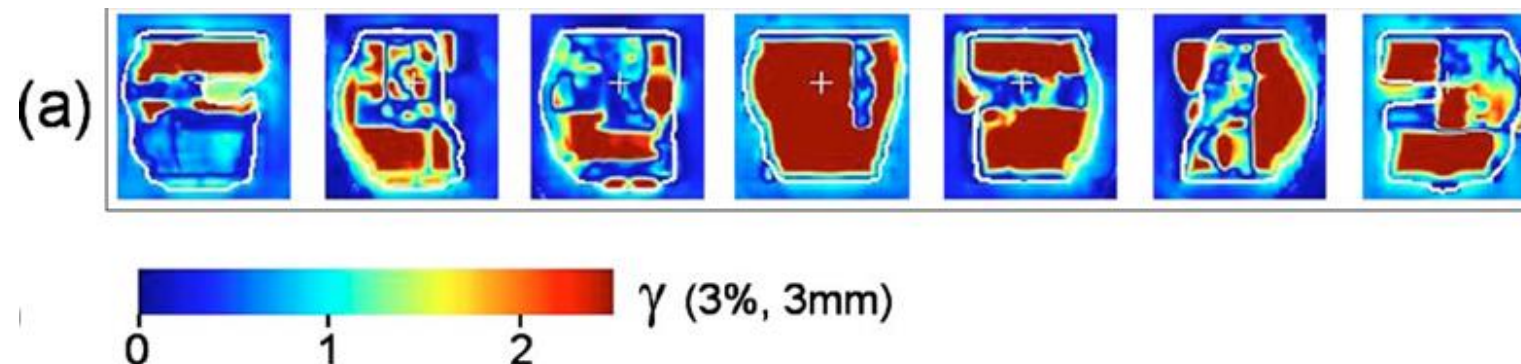


*Mans et al Radiother. Oncol 2010.
McCurdy et al Medical Physics 2009

Case Study

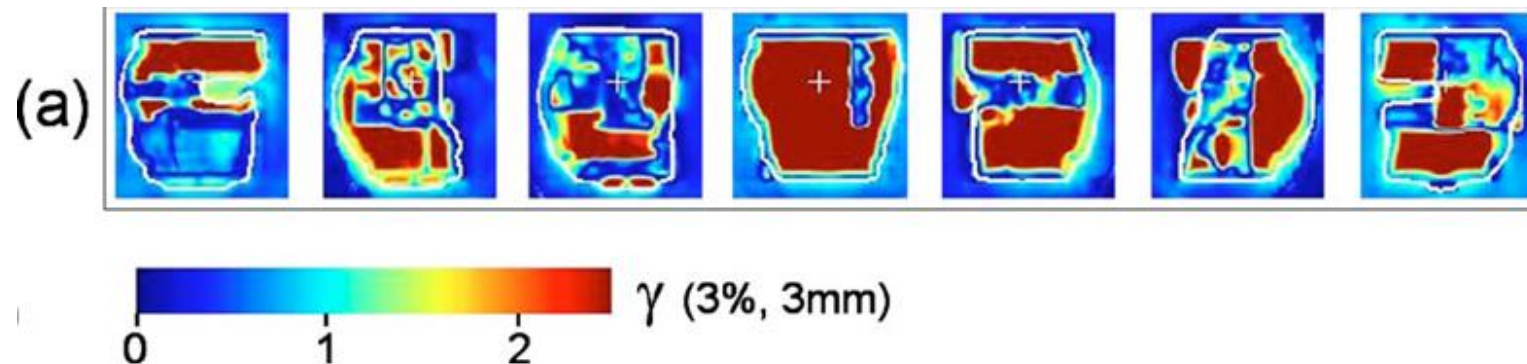
○ Rectum cancer patient (NKI)

- Prescribed 25 Gy to target volume in 5 fractions.
- 7 IMRT beams
- Plan transferred to Mosaik, all protocols followed, no abnormalities observed. Majority of control points corrupted (27 out of 35)
- MLC positions and jaw positions mismatched



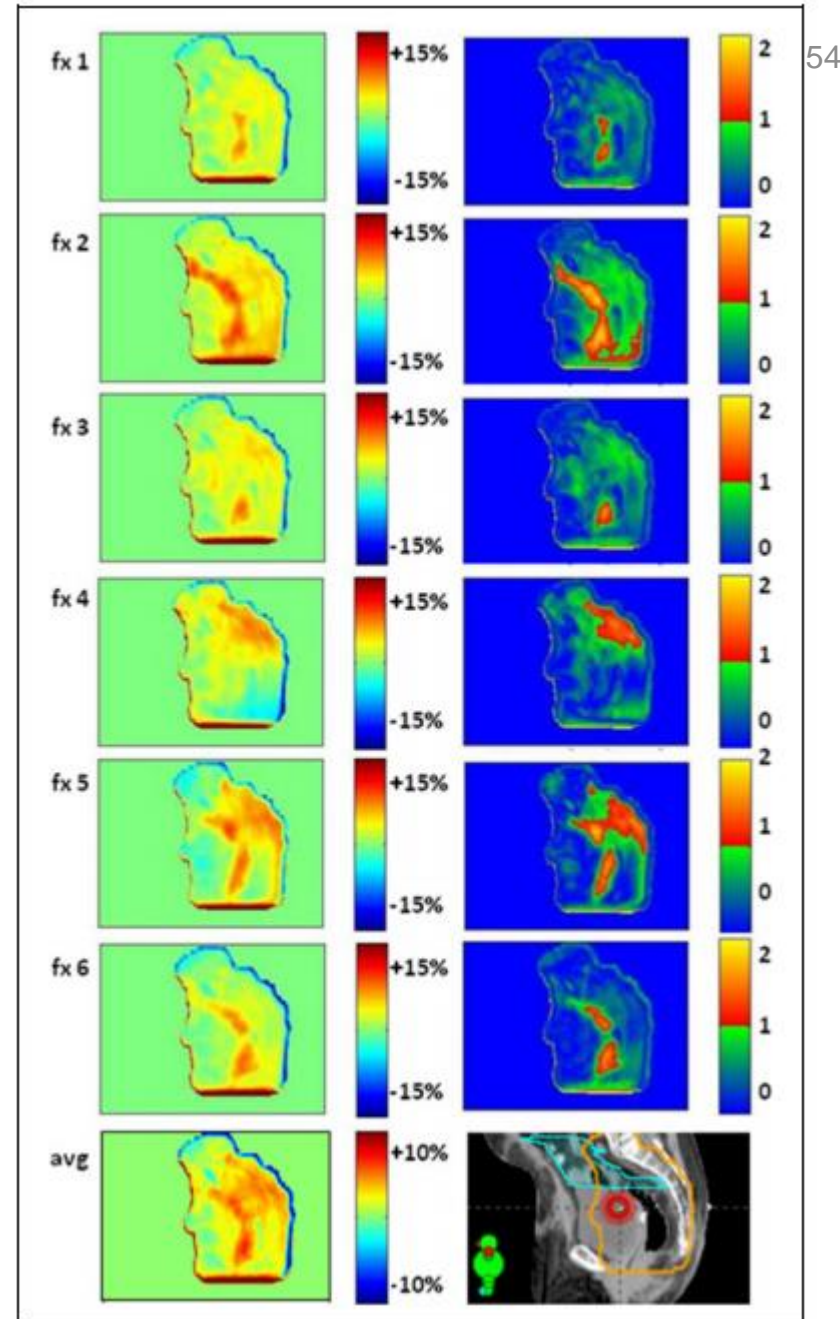
Case Study

- EPID dosimetry done during first fraction, analysis done after first fraction
- Would have been detected pre-treatment
- EPID data used to reconstruct dose, used to inform decisions on continuation of plan



Rectum

- Prone rectal treatments
 - Reconstruction of planar dose at isocenter.
 - Persistent bowel gas, changes to bowel dose



Automation: Maastr

- 3D dose reconstruction using kv CBCT image. 3D portal dose compared to planned dose. Automatically flagged if gamma criteria is not passed.
- 3D calculated for all patients.
- Study done on atelectasis adaptive protocol
 - If significant change observed CTV is re-delineated on CBCT.
 - Discrepancies and changes over time for lung cancer treatments.

